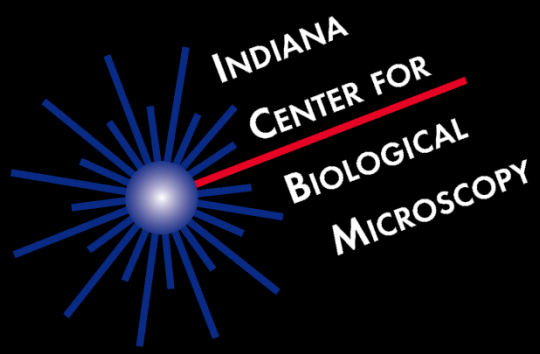
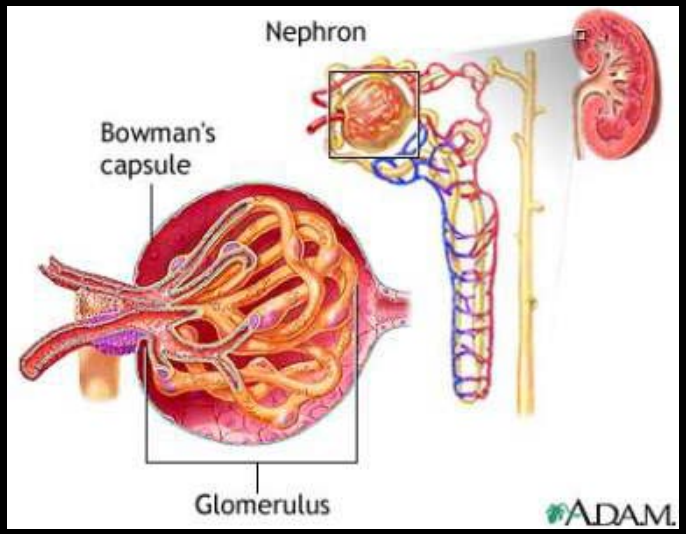
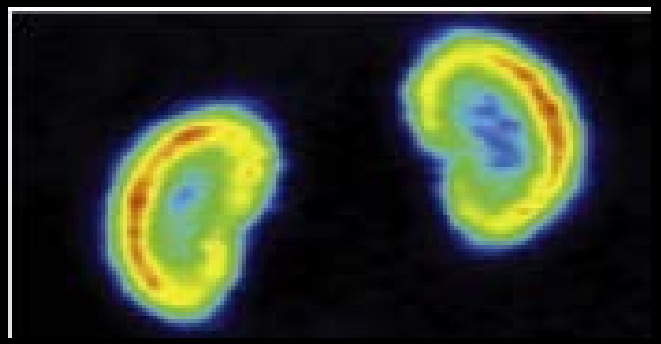


Intravital multiphoton microscopy – Principles and challenges

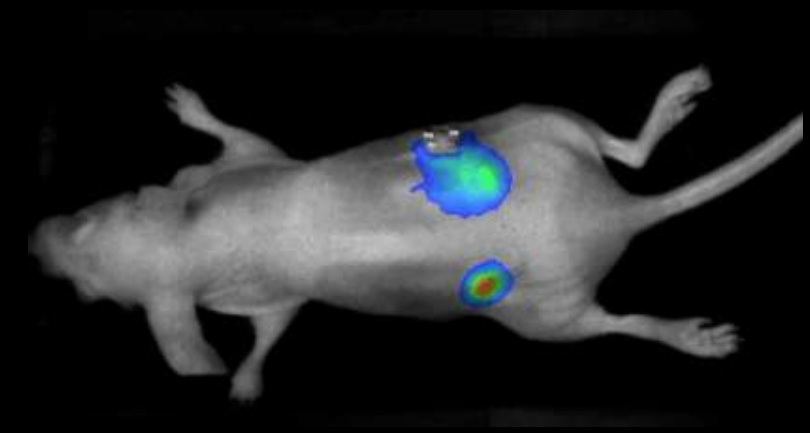
Ken Dunn, PhD
Scientific Director
Indiana Center for Biological Microscopy
Indiana University Medical Center

In vivo imaging of the kidney

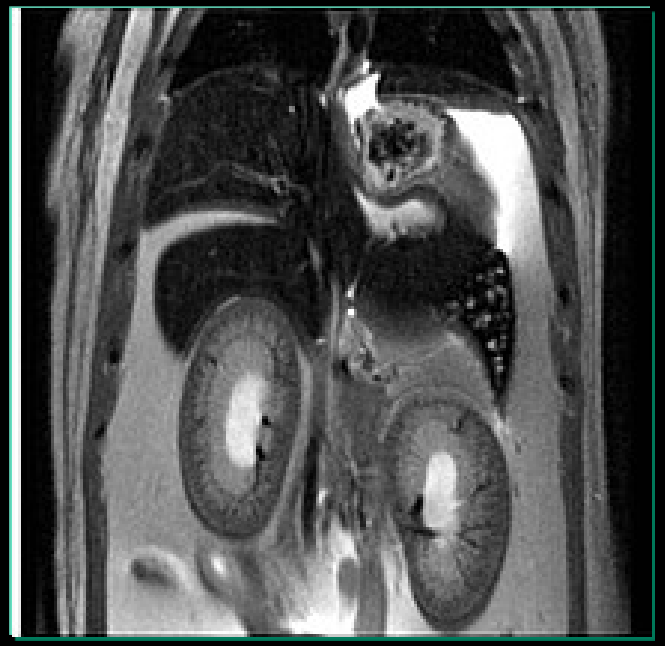




PET
Ceccarini et al., 2009 Cell Metab.

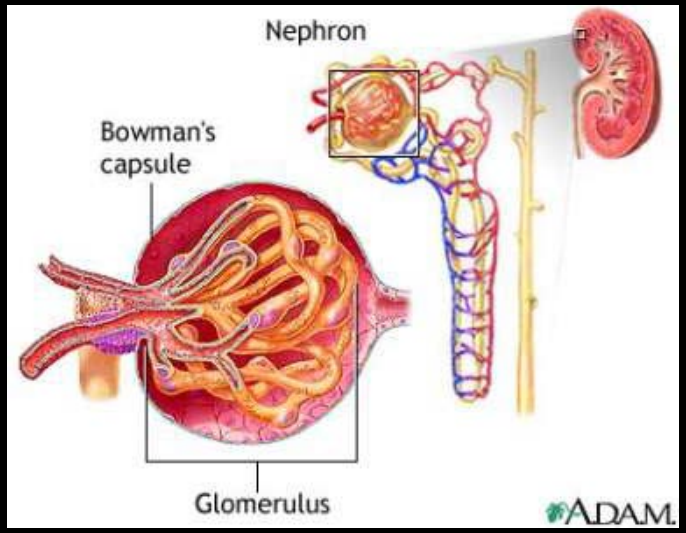


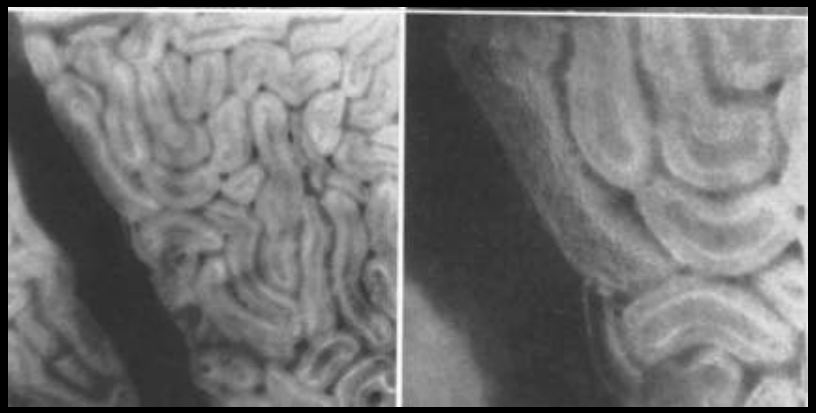
Bioluminescence
Que, Kajizel and Löwik, LUMC, Netherlands



MRI
Bruker Biospin

Intravital microscopy of the kidney





Wide-field microscopy
Steinhausen et al., 1963.

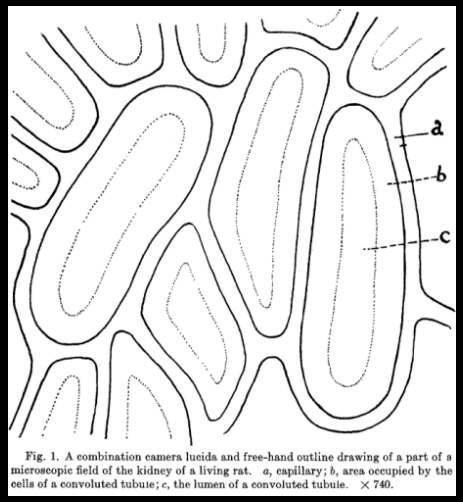
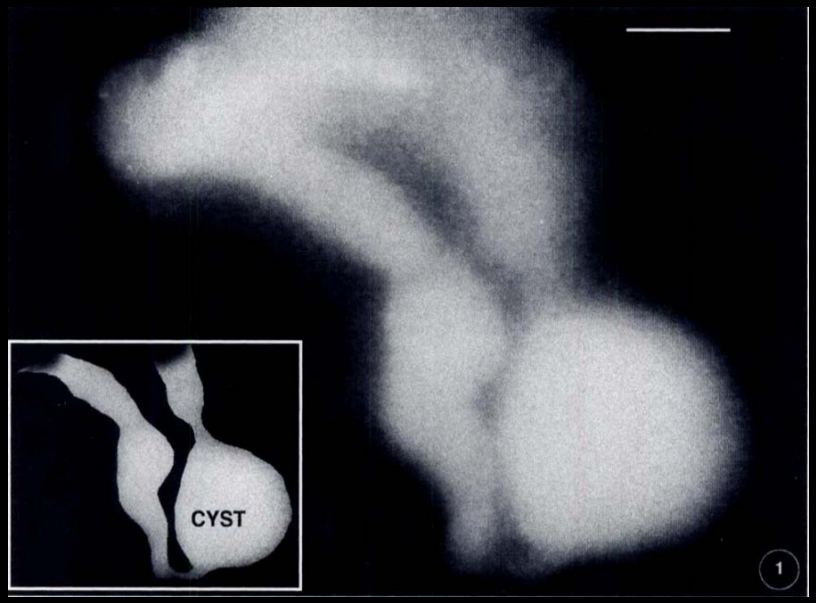


Fig. 1. A combination camera lucida and free-hand outline drawing of a part of a microscopic field of the kidney of a living rat. *a*, capillary; *b*, area occupied by the cells of a convoluted tubule; *c*, the lumen of a convoluted tubule. × 740.

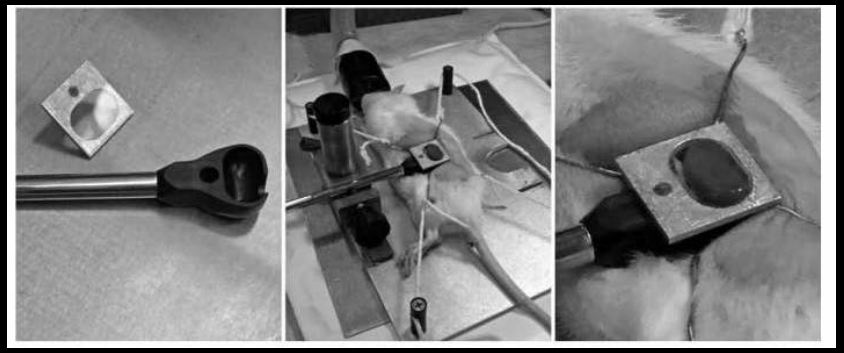
Wide field microscopy
Edwards and Marshall, 1924

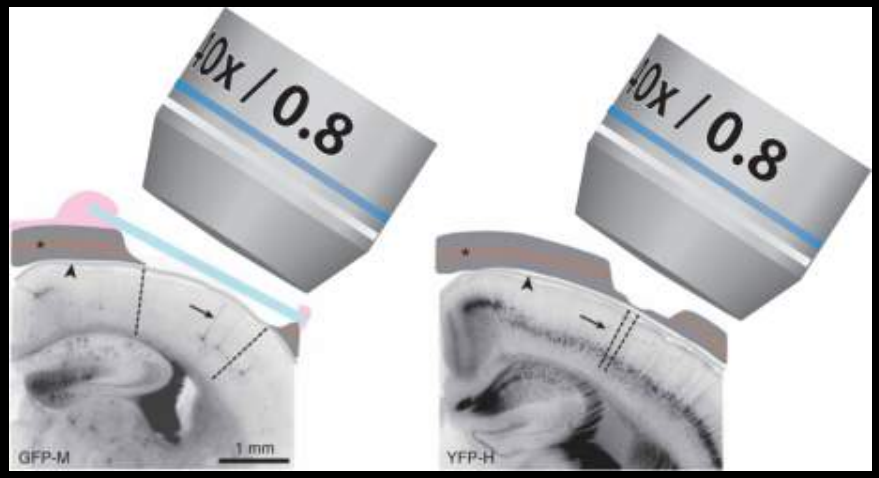


Fluorescence microscopy
Tanner et al., 1997, JASN

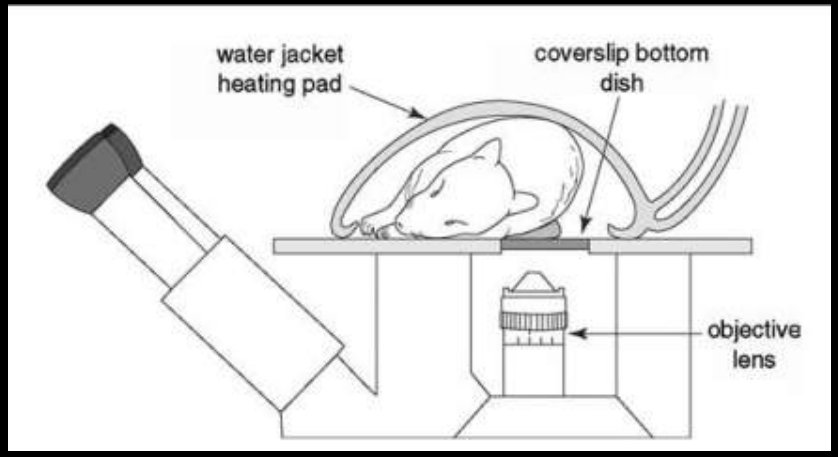
Optical access to tissues in vivo

Oslo University Hospital



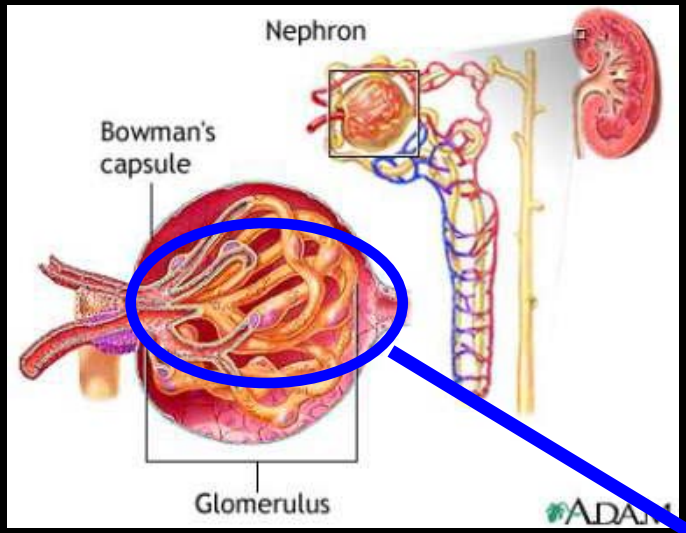


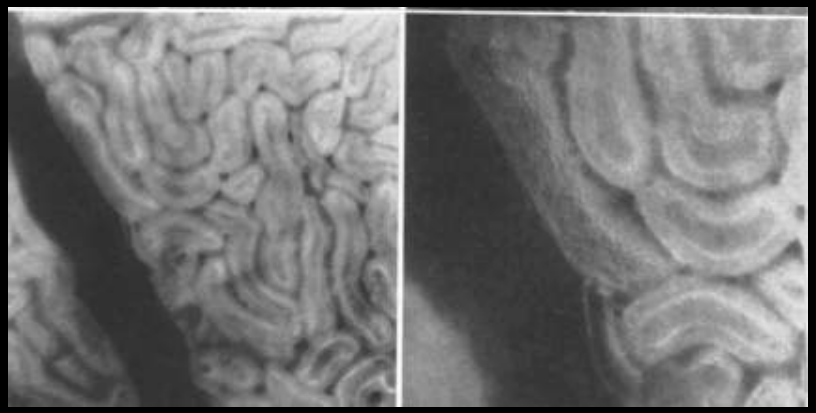
Holtmaat et al. Nature Protocols, 2009



Dunn, Sutton and Sandoval. 2007. Curr. Protocols Cytometry. 12.9.1-12.9.18

Intravital microscopy of the kidney





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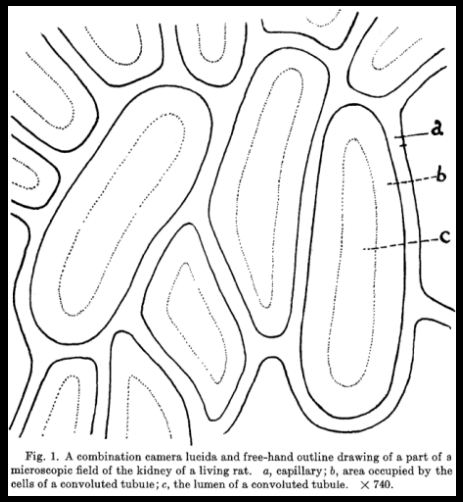

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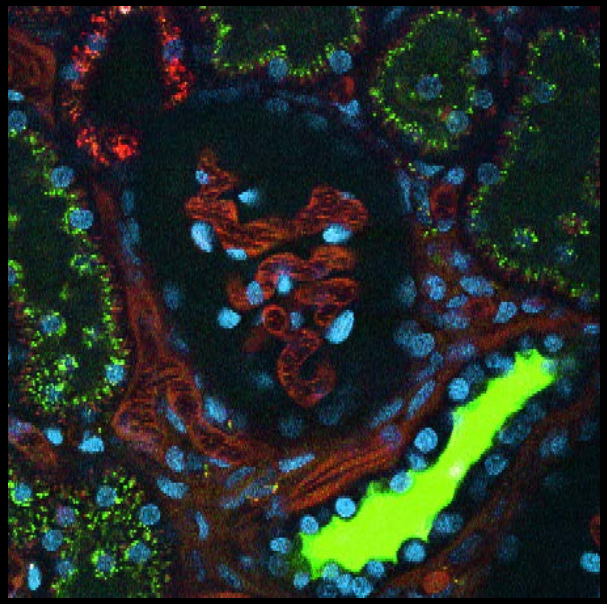
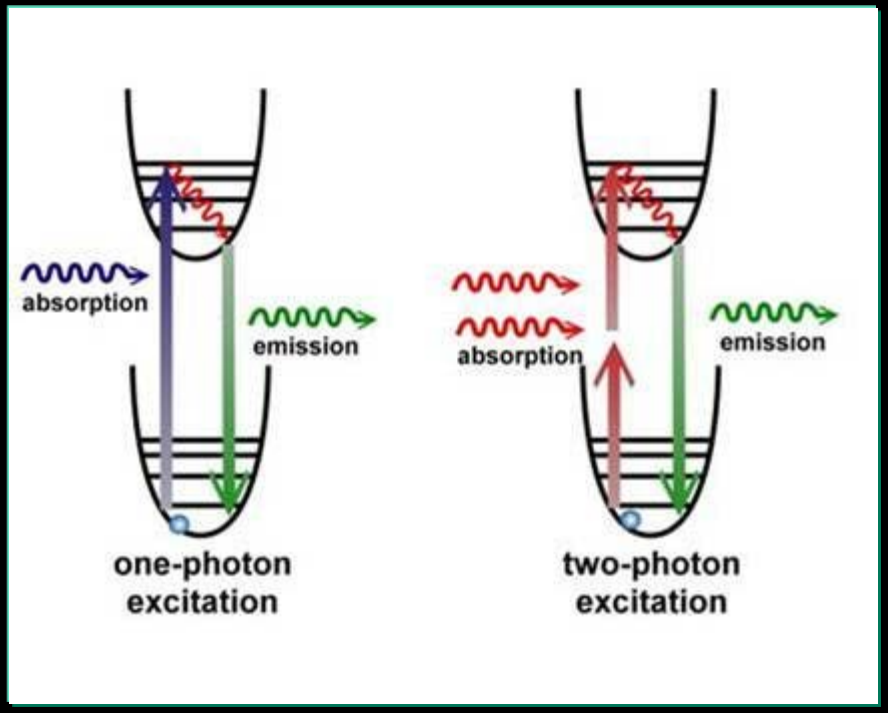


Dunn, Sandoval and Molitoris. 2003. Intravital imaging of the kidney using multiparameter multiphoton microscopy Nephron. 94:e7-11

Multiphoton fluorescence excitation



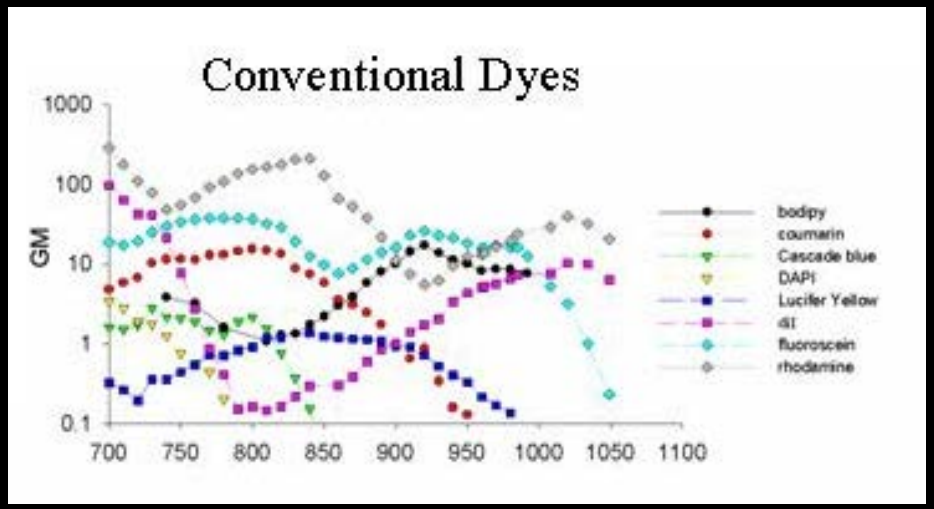
Biophotonics Imaging Lab, Univ. Illinois Urbana-Champaign

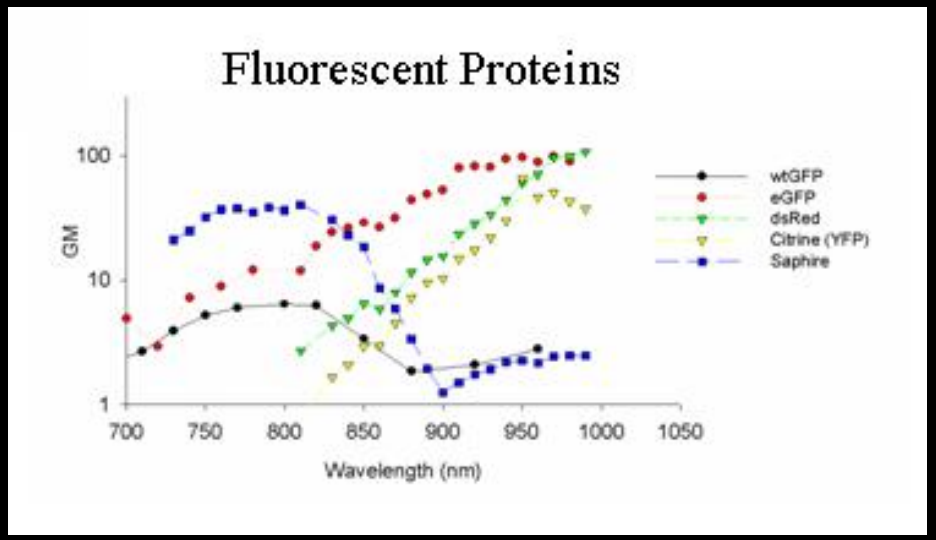
Fluorescence can be stimulated by the absorption of one photon of a particular energy level.

Maria Goppert-Mayer, 1931 –

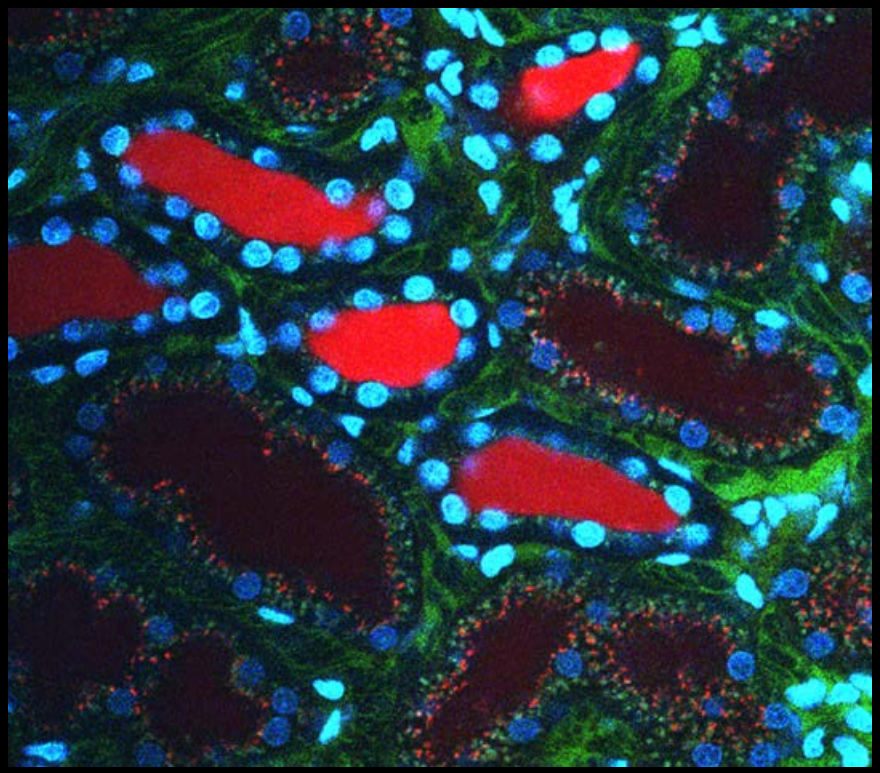
Fluorescence can also be stimulated by the simultaneous absorption of multiple, low-energy photons

Two-photon action cross sections





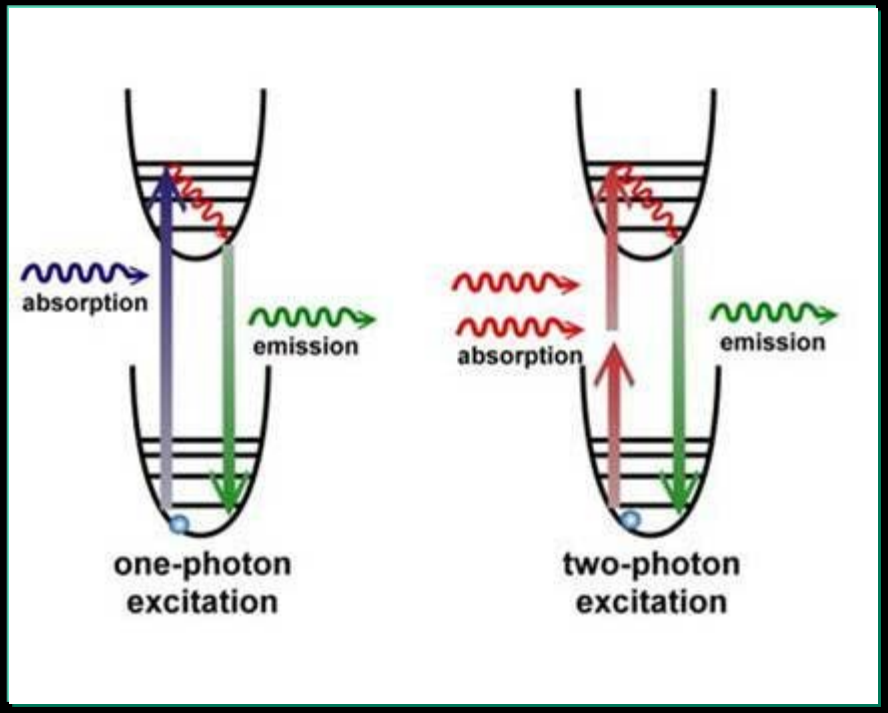
Developmental Resource for Biophysical Imaging Opto-electronics, Cornell
(Watt Webb and Warren Zipfel)



10 kD Rhodamine Dextran,
500 kD Fluorescein Dextrn
Hoechst 33342

Dunn et al., 2002. AJP Cell. 283:C905-C916

Multiphoton fluorescence excitation Requires an enormous density of photons



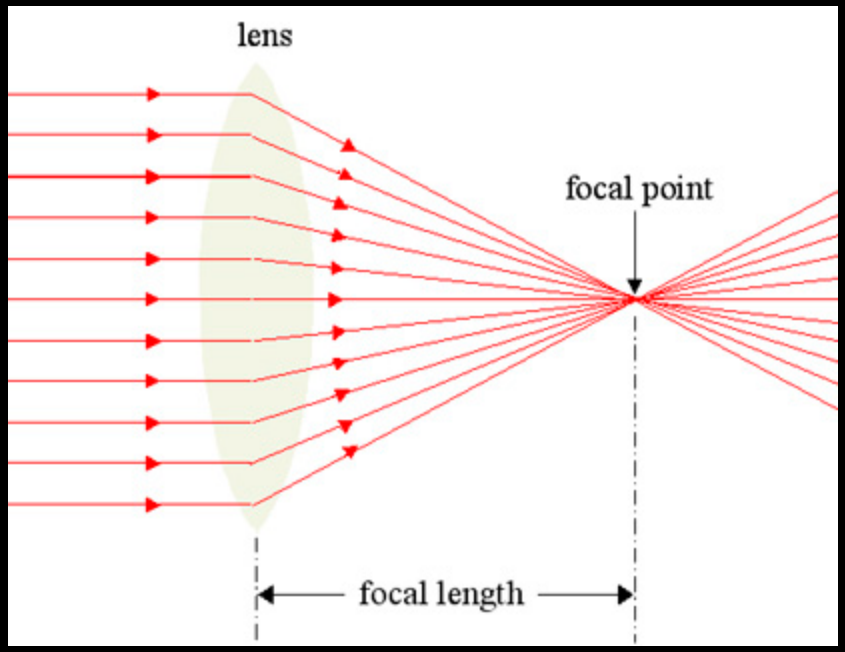
Biophotonics Imaging Lab, Univ. Illinois Urbana-Champaign

"Simultaneous absorption of two photons" – within ~ 10 attoseconds (10^{-17} seconds)

Detectible two-photon fluorescence excitation requires peak power on the order of 200 GW/cm^2
~ 300,000x the surface of the sun

Two photon fluorescence excitation first demonstrated with development of the ruby laser – Kaiser and Garrett, 1961

Multiphoton fluorescence excitation Requires an enormous density of photons



DiracDelta Science

Detectible two-photon fluorescence excitation requires peak power on the order of 200 GW/cm^2
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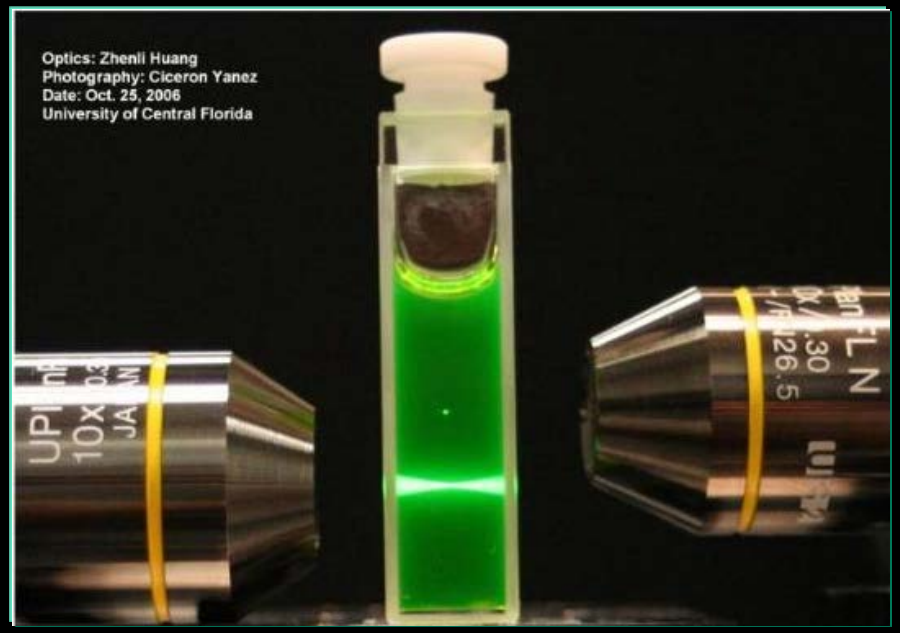
For multiphoton microscopy, this density is provided by focusing laser illumination through high NA objective lenses.

Photon density decreases with the 4th power of distance from the lens focus

Multiphoton fluorescence excitation Requires an enormous density of photons



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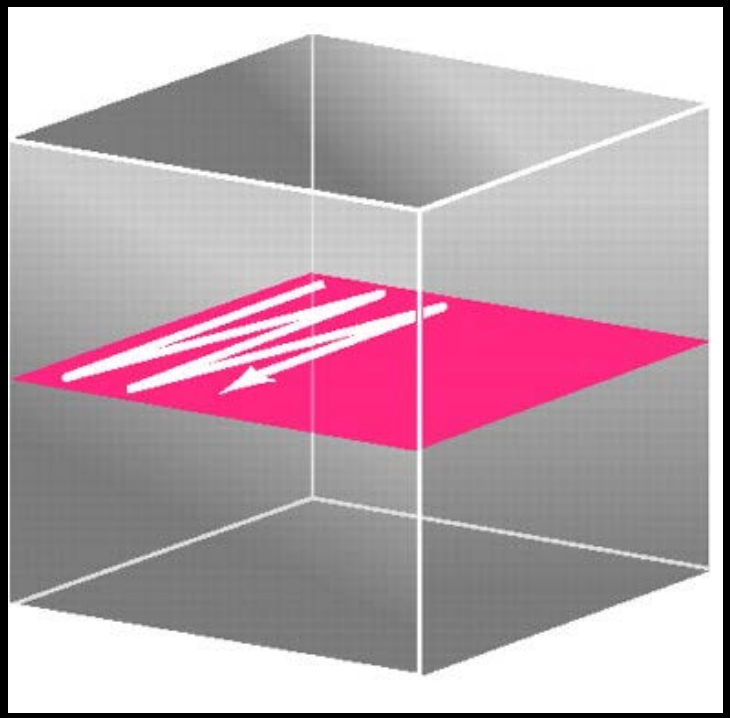
Photon density decreases with the 4th power of distance from the lens focus

Two-photon absorption occurs ONLY in the sub-femtoliter volume at the focus

Multiphoton fluorescence excitation is spatially constrained

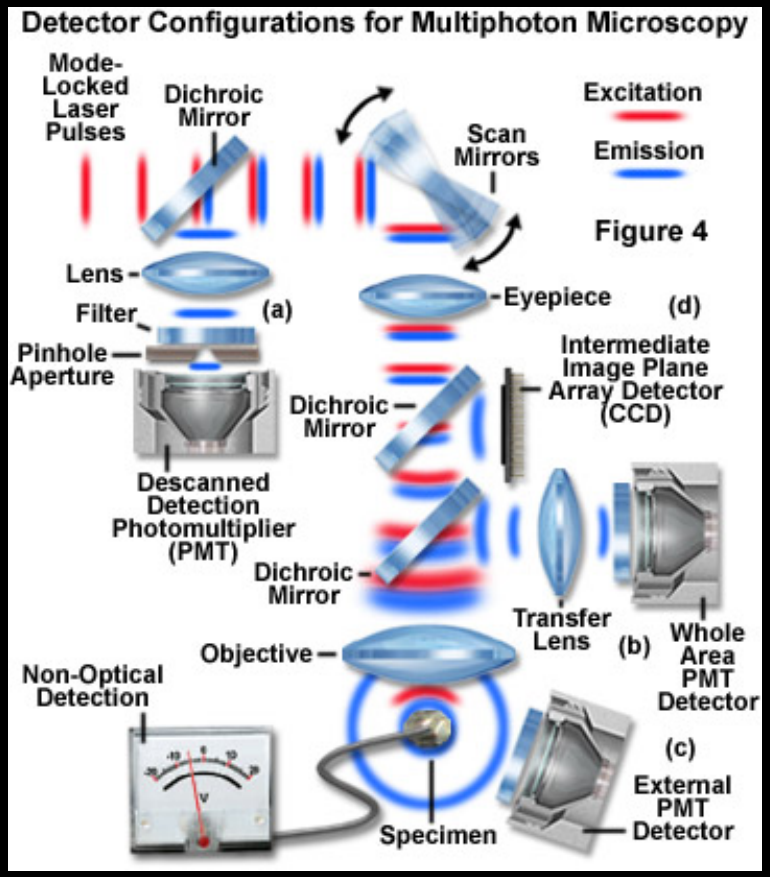


Göbel and Helmchen 2007

Build an image from single points

- A 2D image is formed by raster scanning a laser over the sample
- A 3D image is formed by collecting a set of 2D images at different depths

Multiphoton fluorescence excitation is spatially constrained

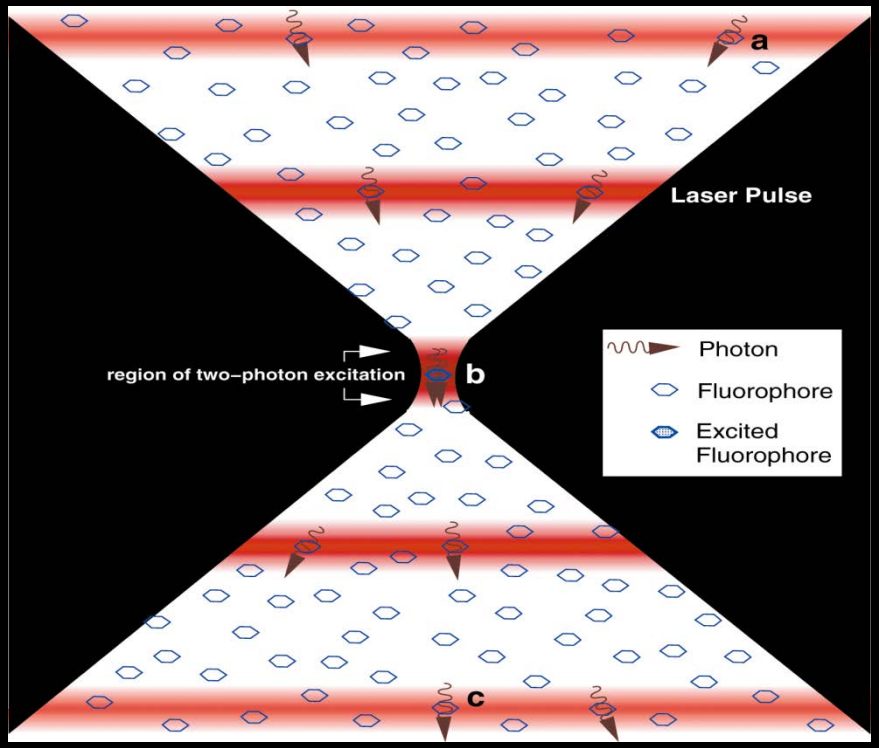


Zipfel et al., 2003

Build an image from single points

- A 2D image is formed by raster scanning a laser over the sample
- A 3D image is formed by collecting a set of 2D images at different depths
- Image is formed by collecting, rather than imaging photons

But 300,000 times brighter than the surface of the sun????



Dave Piston

Denk, Strickler and Webb, 1990

- Use a pulsed laser ~100 femtosecond pulses at a rate of 80 MHz

Peak power sufficient for multiphoton excitation, but average power low enough to minimize damage.

- e.g. 28 mW average provides 200 GW/cm^2 peak with 0.8 NA objective

Note that pulses do not REALLY limit the volume of excitation

- Actually ~ 45 microns long and ~ 4 meters apart

Multiphoton microscope designs

Gregor Lab, Princeton

Leica SP8 MP

Roberto Weigert, Editor of "Intravital"
Building your own 2P microscope system
Thursday, 9:20 am

Ken Dunn
Writing a Shared Instrumentation Grant
Wednesday, 5pm

Fun facts about multiphoton microscopy

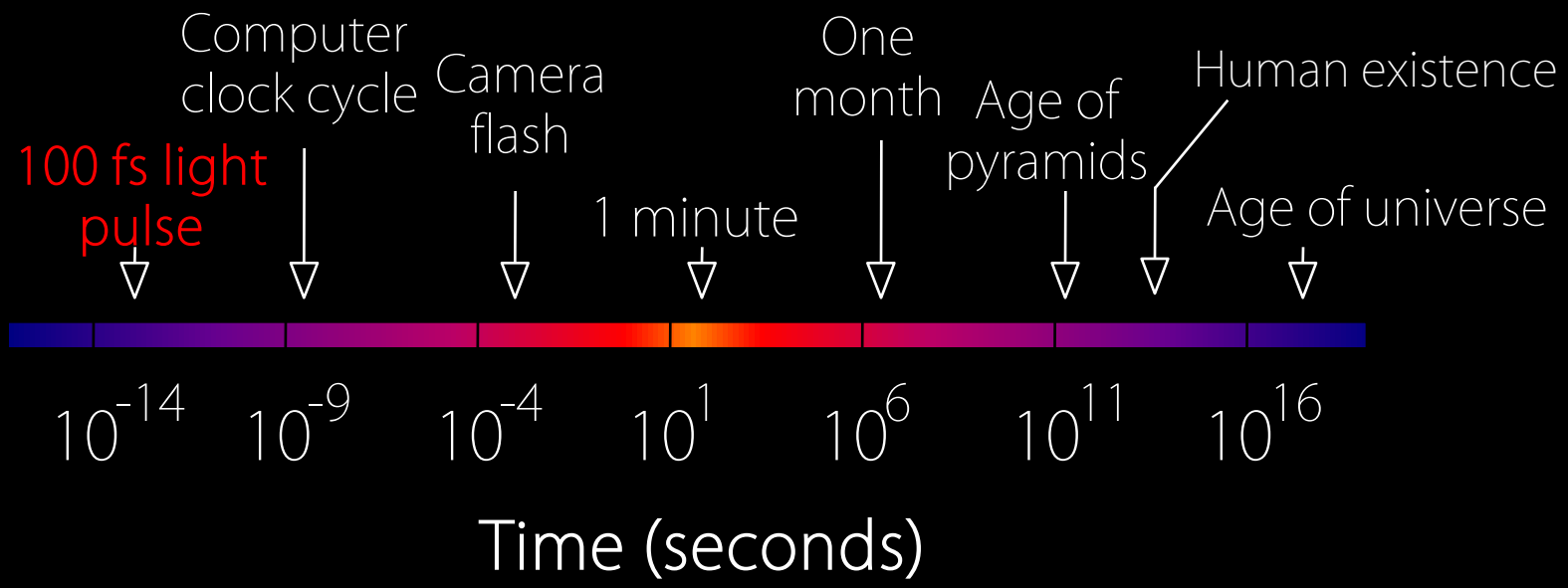
How frequently does multiphoton fluorescence excitation occur outside of a microscope?

Calculations made by Winfried Denk indicate that a molecule of rhodamine B exposed to direct sunlight will experience:

- A one-photon absorption around once per second.
- A two photon absorption once every 10,000 years.
- A three-photon absorption . . . never in the history of the universe.

Fun facts about multiphoton microscopy

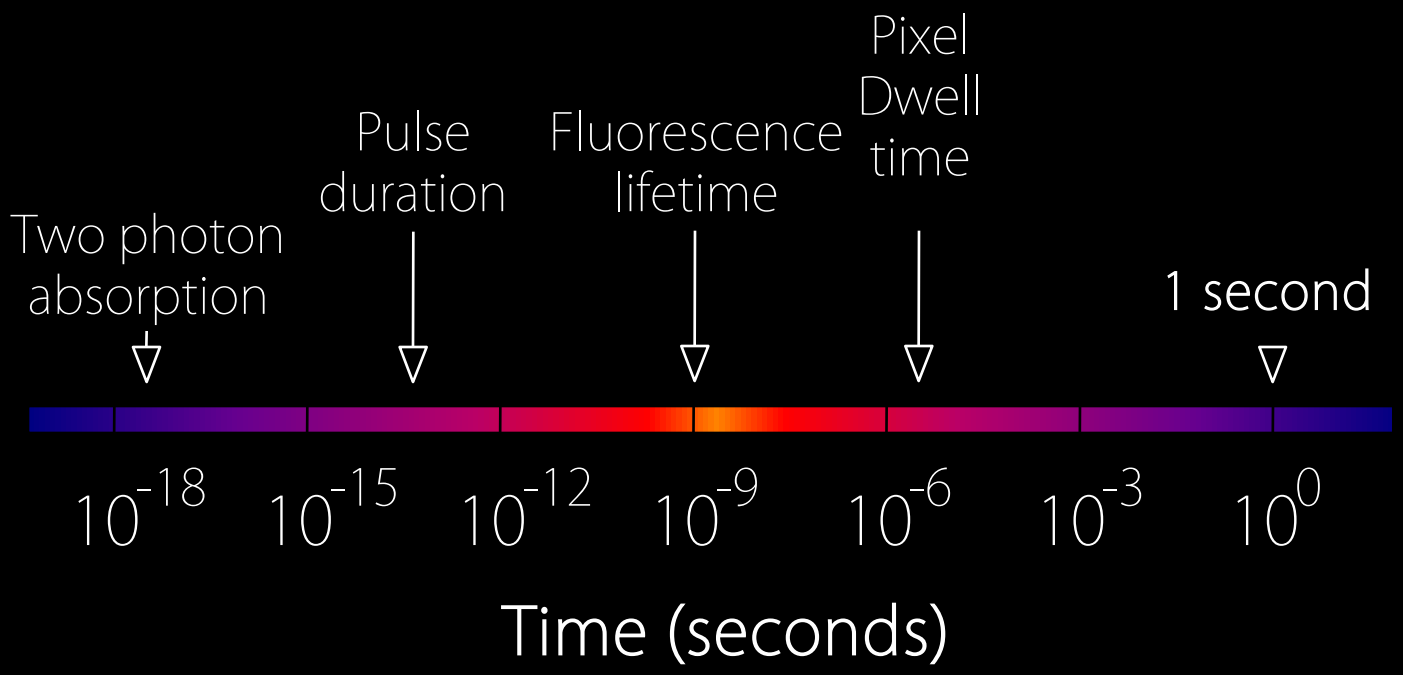
Ridiculous time scales



100 fs is to 10 minutes as 10 minutes is to the age of the universe.

Rick Trebino, University of Georgia

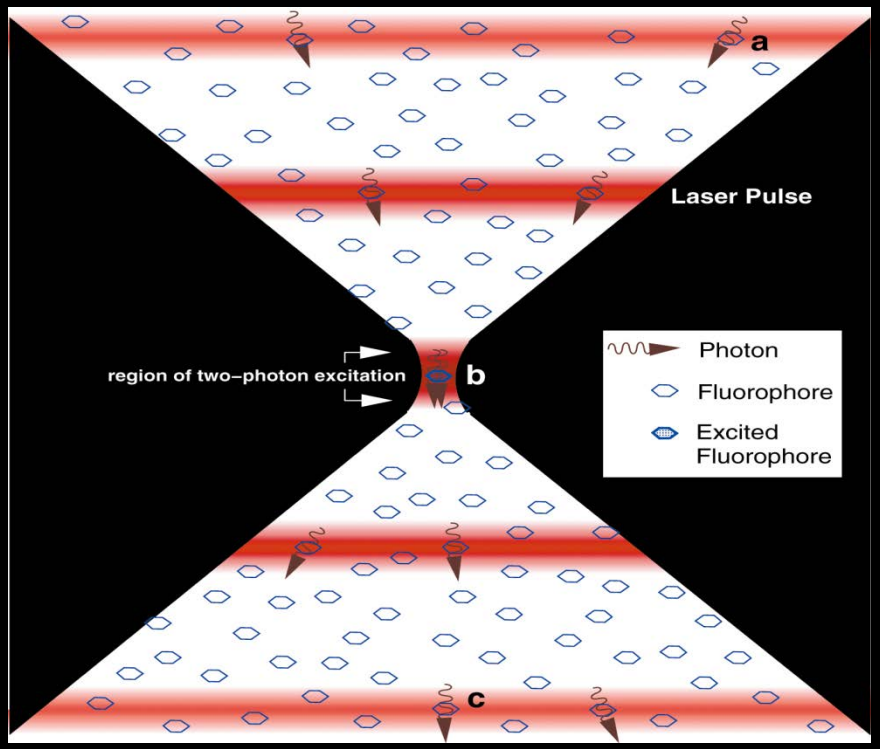
Fun facts about multiphoton microscopy
Relative time scales



- Fluorescence lifetimes are ~ 1 billion times the length of the virtual intermediate state
- At 80 MHz, the laser pulses are spaced ~ 3 fluorescence lifetimes apart (serendipitous)
- A fluorophore will be illuminated ~320 times during a 4 microsecond pixel dwell time

Fun facts about multiphoton microscopy

When the laser is on, it's mostly off



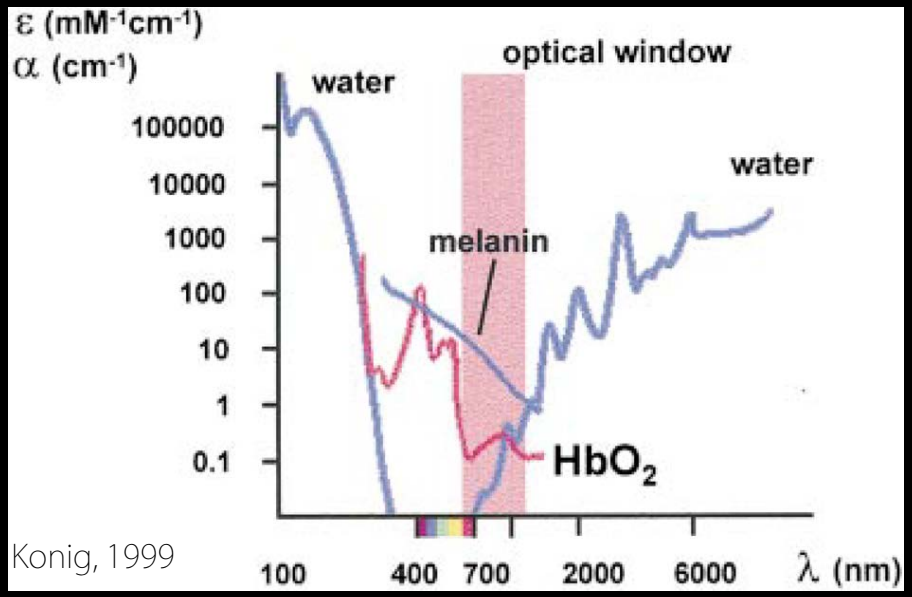
Dave Piston

- The sample is illuminated with 100 femtosecond pulses at a rate of 80 million times per second - 0.001% of the time
  - This duty cycle is equivalent to a one second pulse occurring once a day.

Why multiphoton microscopy?

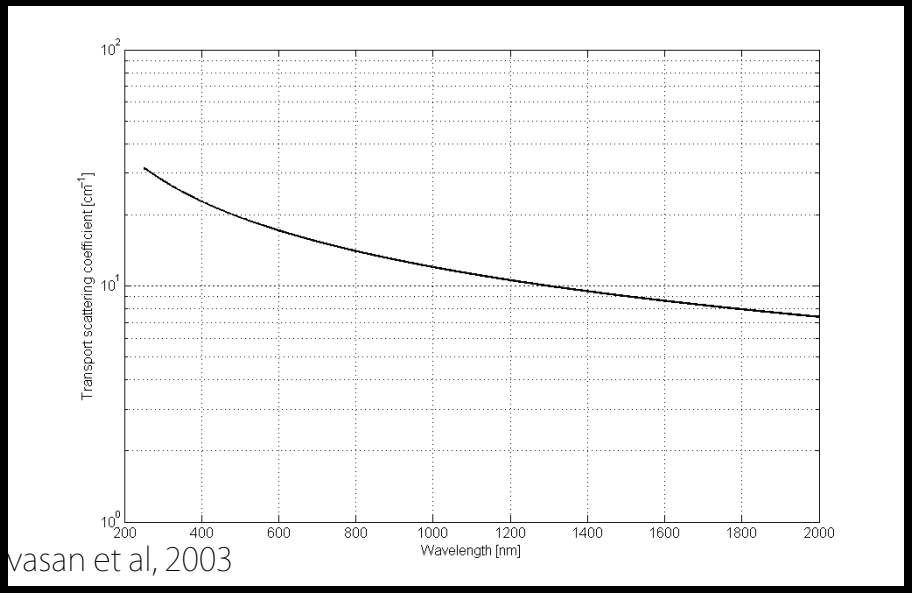
Complex
Expensive
Poorer resolution

Why multiphoton microscopy?



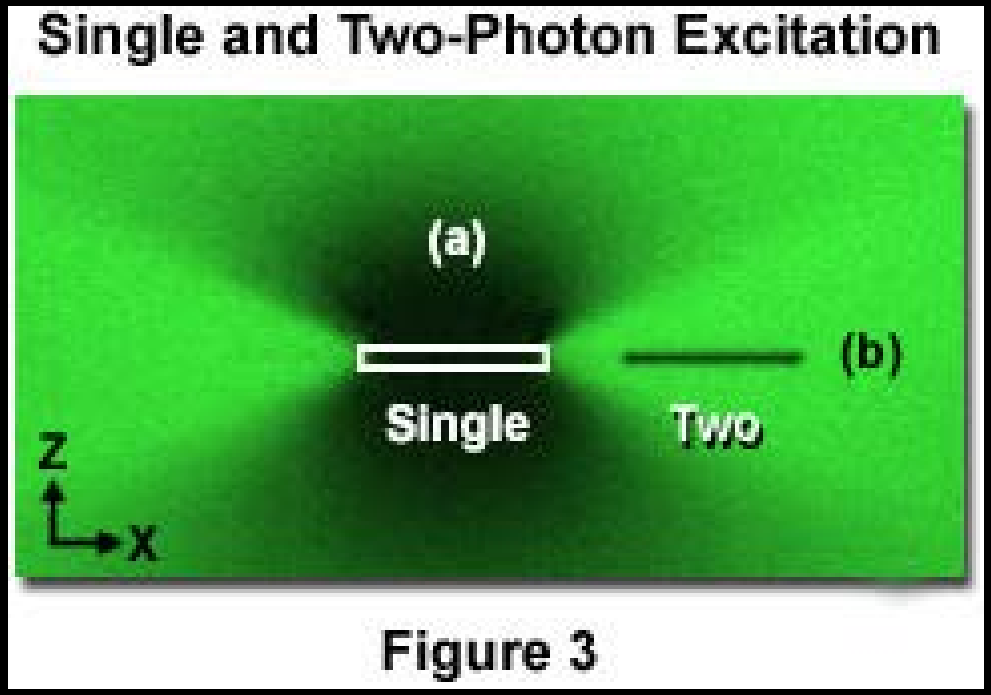
Konig, 1999

- IR light penetrates deeper, with less damage



vasan et al, 2003

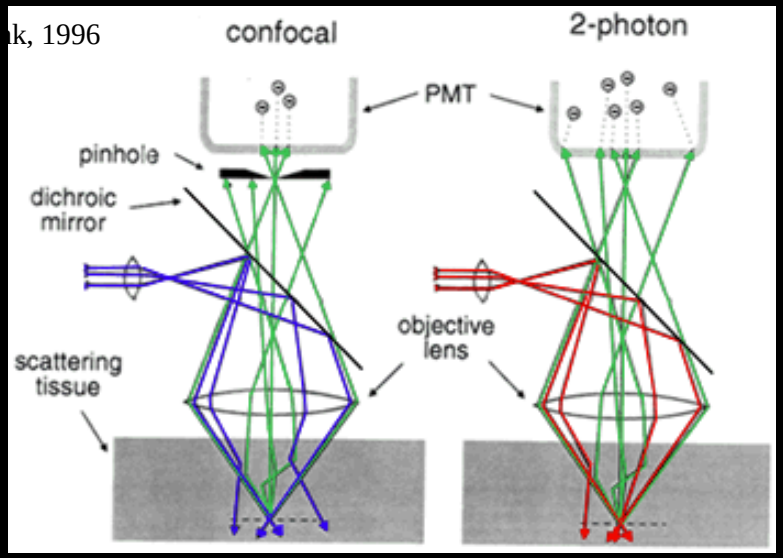
Why multiphoton microscopy?

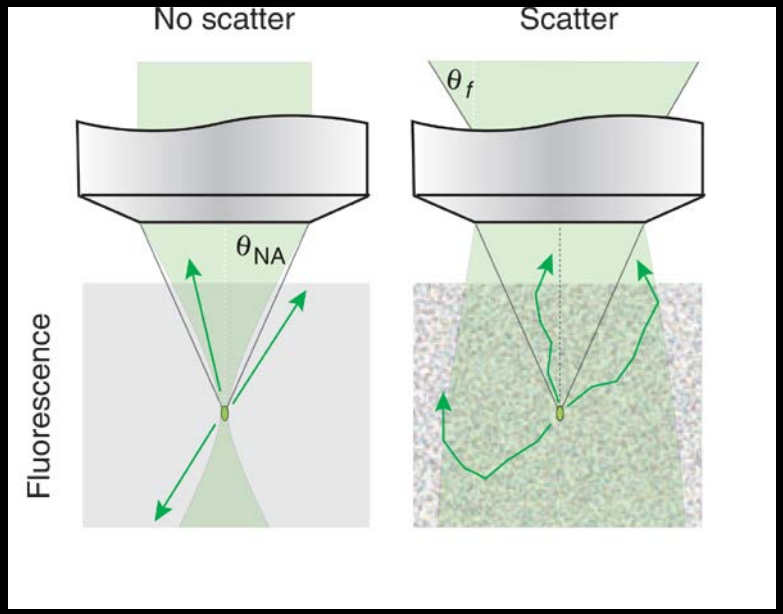


Nikon MicroscopyU

- IR light penetrates deeper, with less damage
- Photobleaching only in the focal plane (but more of it)

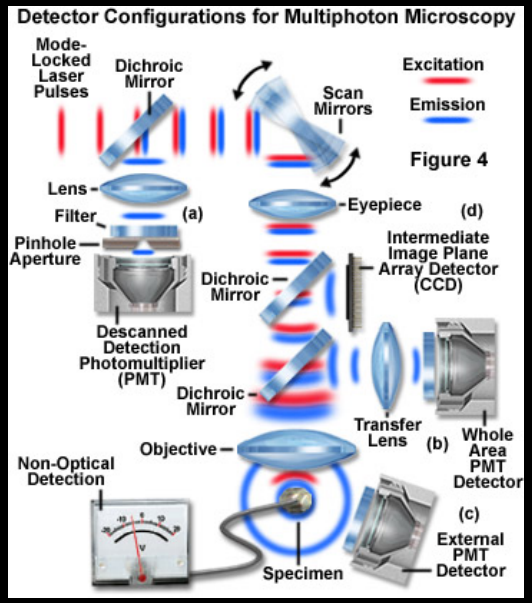
Why multiphoton microscopy?

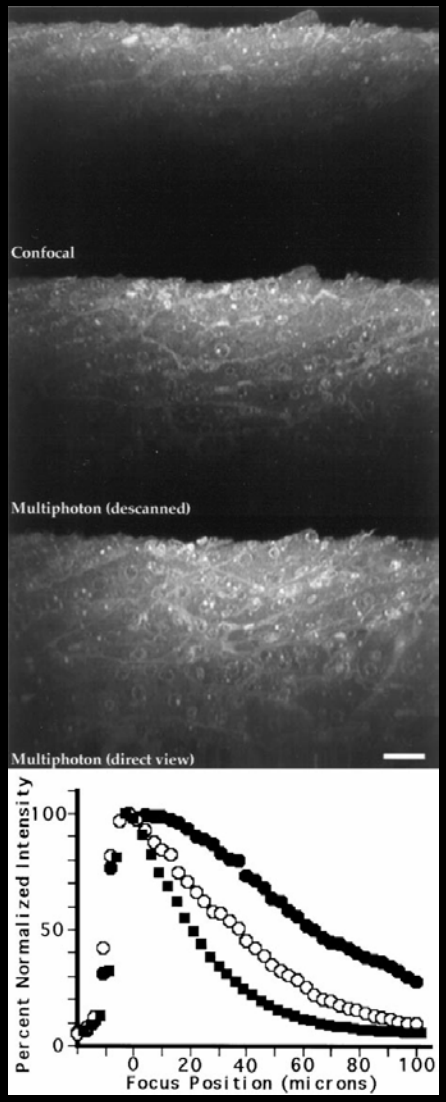




- IR light penetrates deeper, with less damage
- Photobleaching only in the focal plane (but more of it)
- Optical sectioning without an emission aperture - less loss to scattering

Why multiphoton microscopy?





Centonze and White, 1998

- IR light penetrates deeper, with less damage
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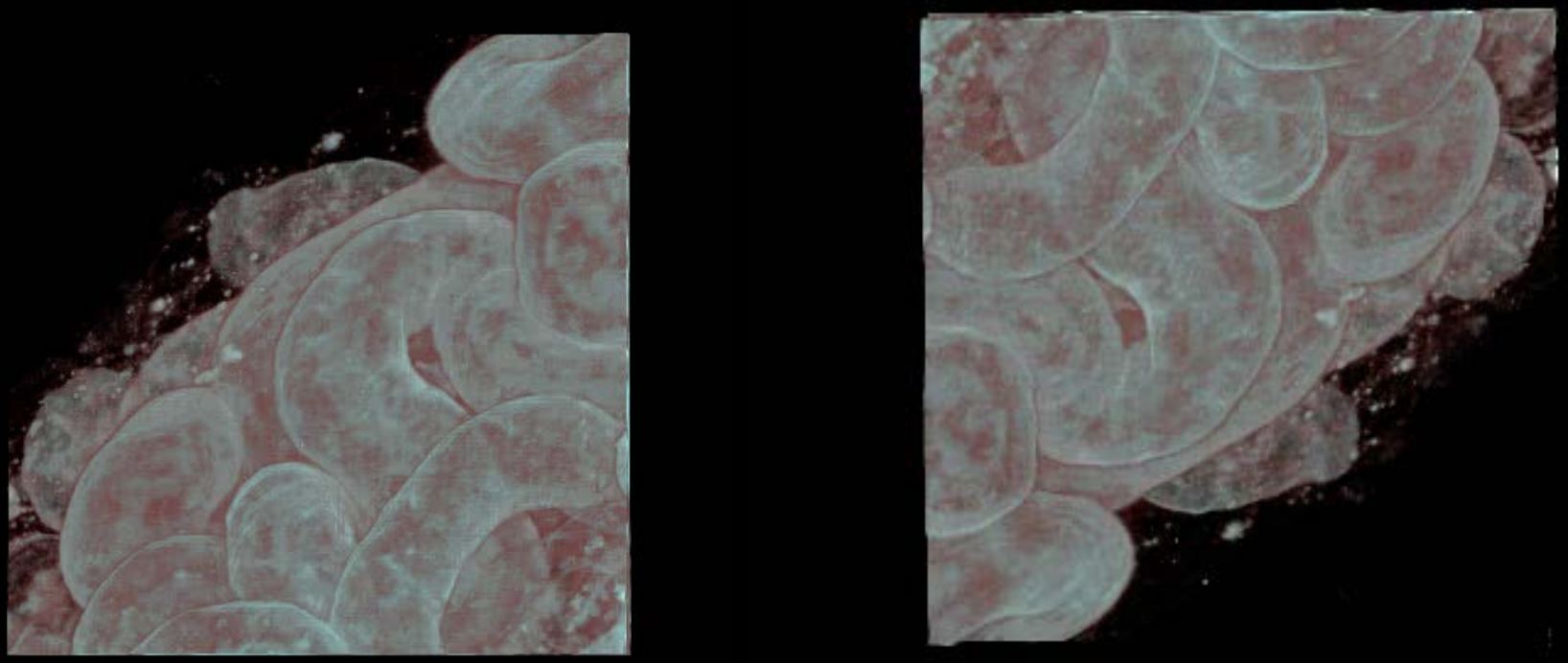
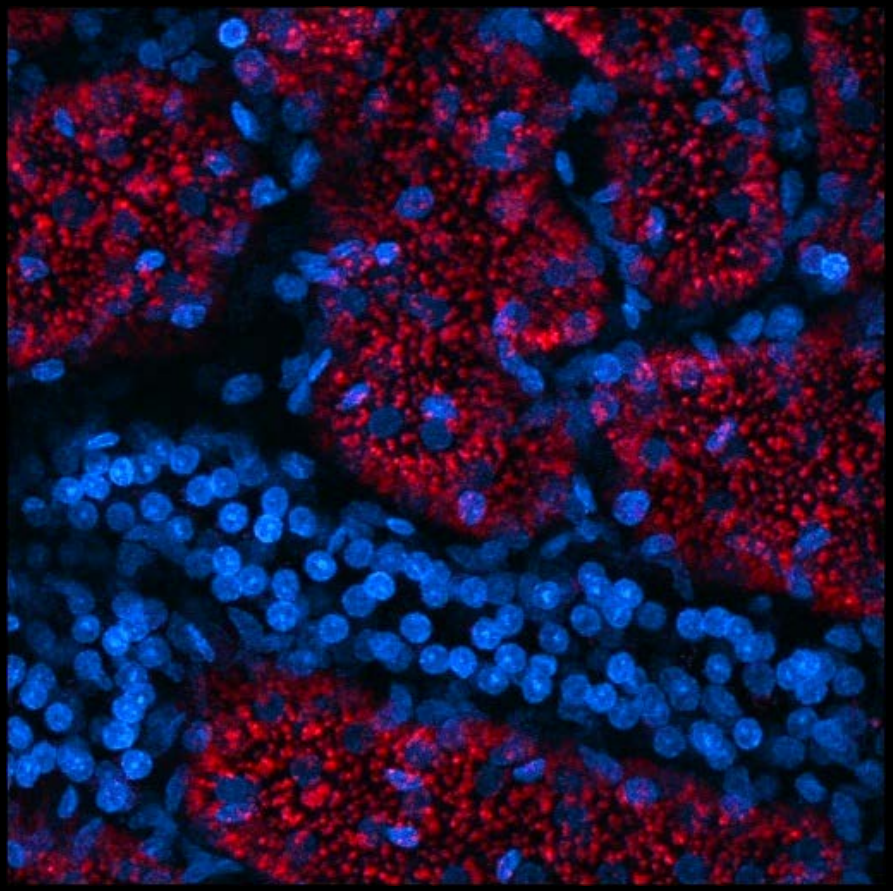
Why multi-photon microscopy? Deep-tissue imaging at high resolution



120 micron thick volume of mouse embryonic kidney
- Carrie Phillips, Nephrology

Why multi-photon microscopy? Intravital microscopy



- Intravital microscopy provides submicron resolution and nanomolar sensitivity in under a second.
- Multiphoton microscopy has extended the reach of intravital microscopy to the scale of tissues and the functional components of organs.

Applications of intravital multiphoton microscopy in biomedical research

Brain function and pathology
- Neural development and activity - Winfried Denk, Karel Svoboda
- Alzheimer's disease - Brian Bacskai, Brad Hyman
- Astrocyte-neuron signaling - Jan Nedergard
- Vascular function in the brain - David Kleinfeld

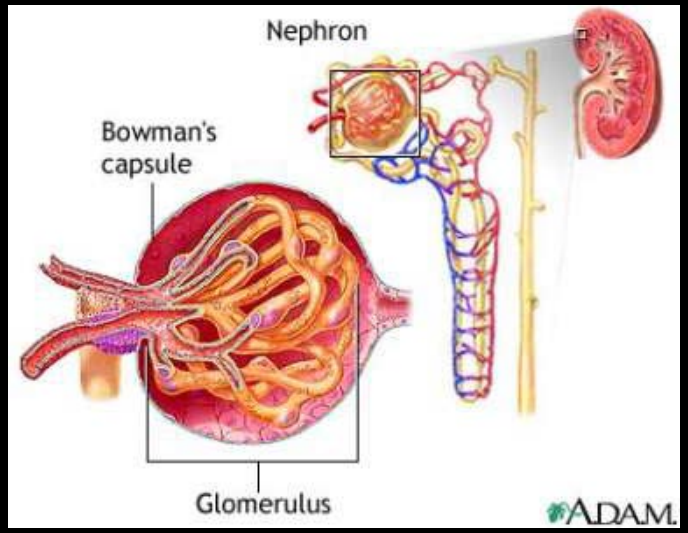
Tumor biology
- Tumor cell dynamics and metastasis - John Condelis, John Segal
- Angiogenesis/vascular function, gene expression - Rakesh Jain

Immunology
- T-cell interactions and dynamics- Michael Dustin, Ullrich Von Andrian, Michael Cahalan
- Immune surveillance in the brain - Fritjof Helmchen, W.B. Gan

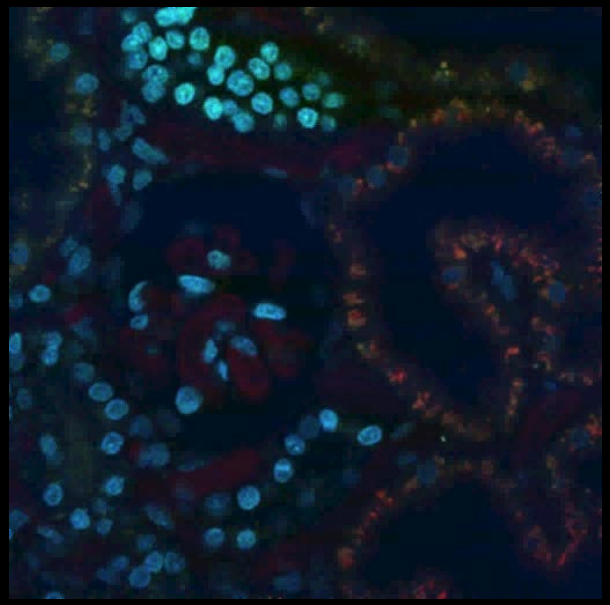
Liver function
- Mitochondria and liver injury - John Lemasters
- In vivo analysis of hepatobiliary transport – Ken Dunn

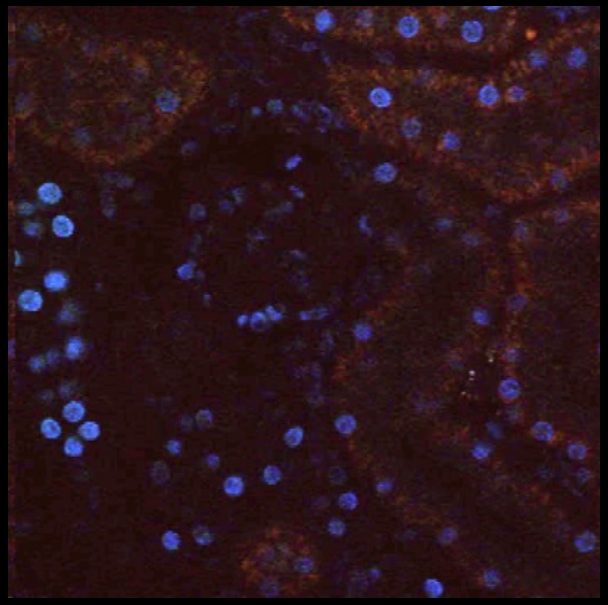
Kidney function
- Pathology and treatment of renal ischemia - Bruce Molitoris
- Pathobiology of AKI - Katherine Kelly
- Renal septic injury - Pierre Dagher
- Microvascular function in renal injury - Tim Sutton
- Glomerular function - Janos Peti-Peterdi

Roberto Weigert, Editor of "Intravital"
IVM studies of membrane transport in salivary gland
Tuesday, 5pm



Dynamic intravital microscopy of the kidney



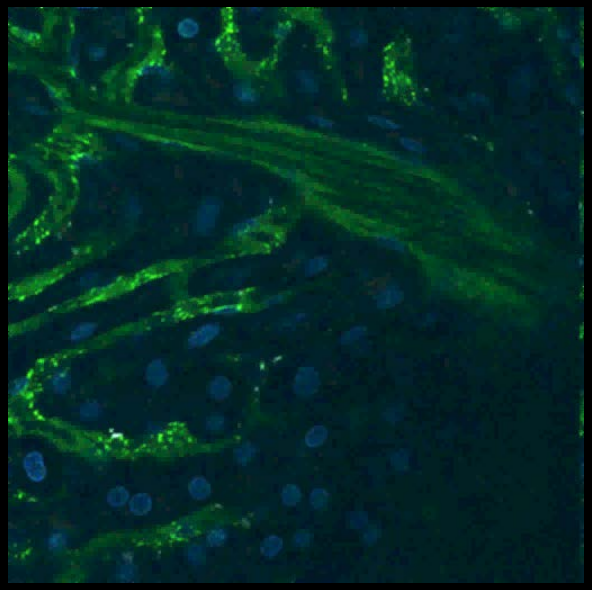


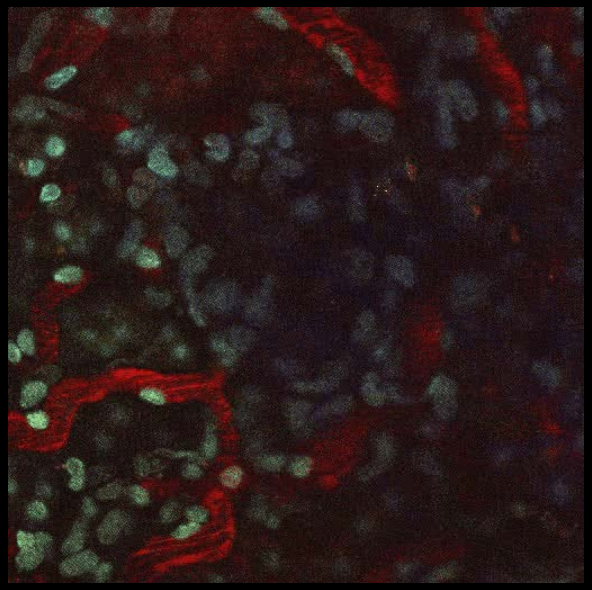
Ruben Sandoval and Bruce Molitoris

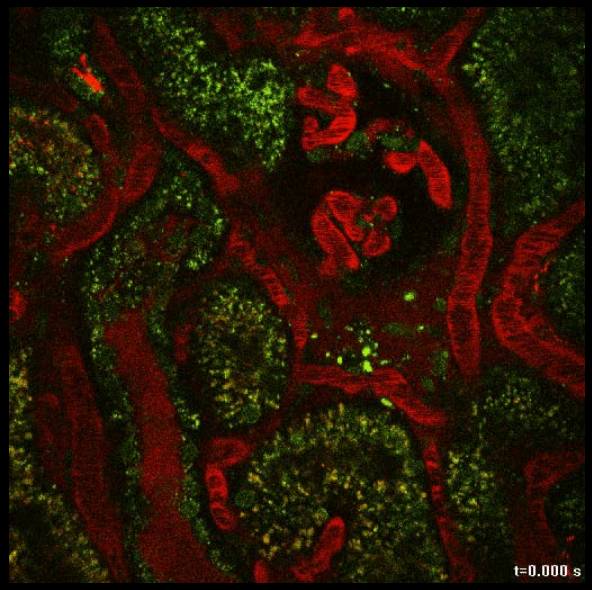
Challenges of subcellular imaging in living animals

- Motion artifacts from respiration and heartbeat

Motion artifacts in intravital microscopy

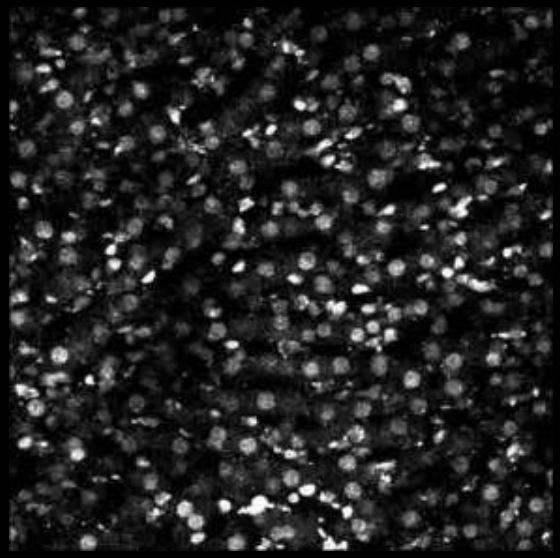




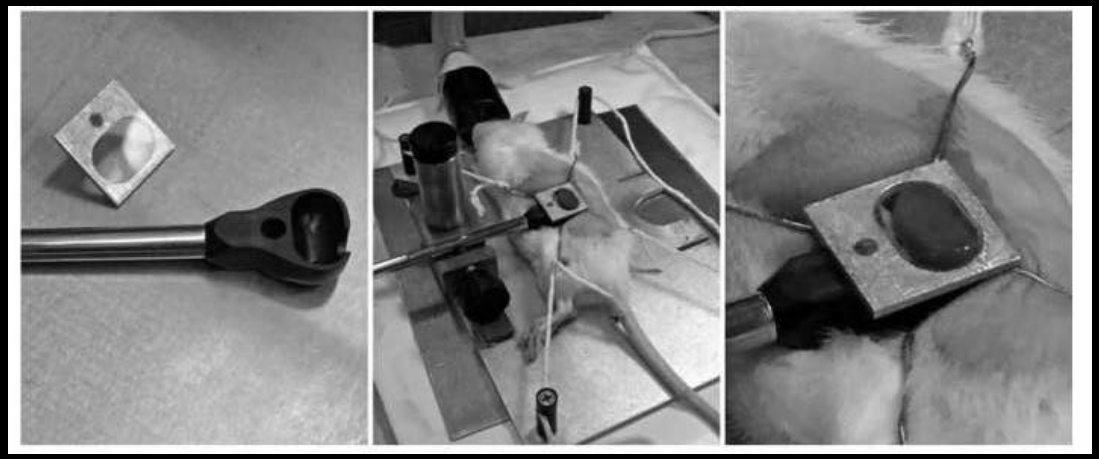


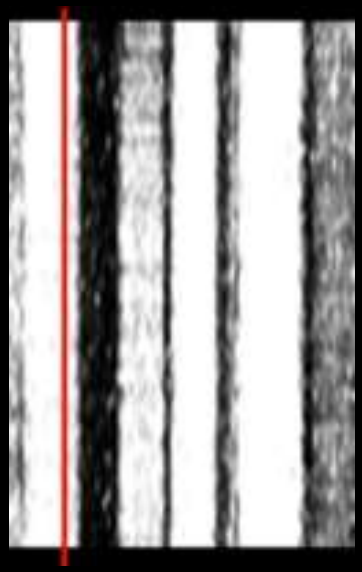
Kang, et al. 2006. AJP Renal

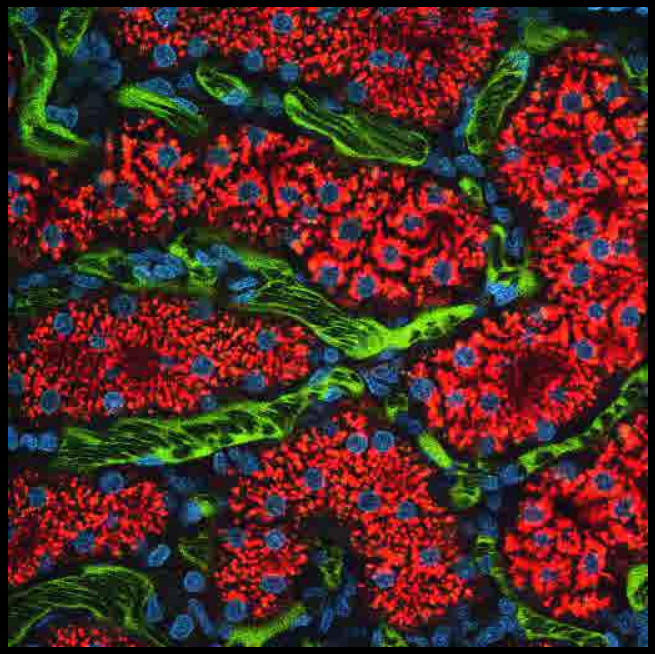
Reducing motion artifacts in intravital microscopy - Immobilize the organ



75 images collected over 30 min

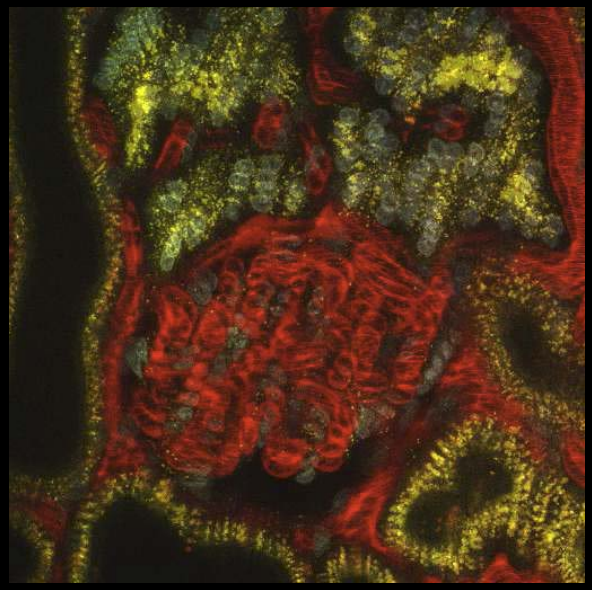




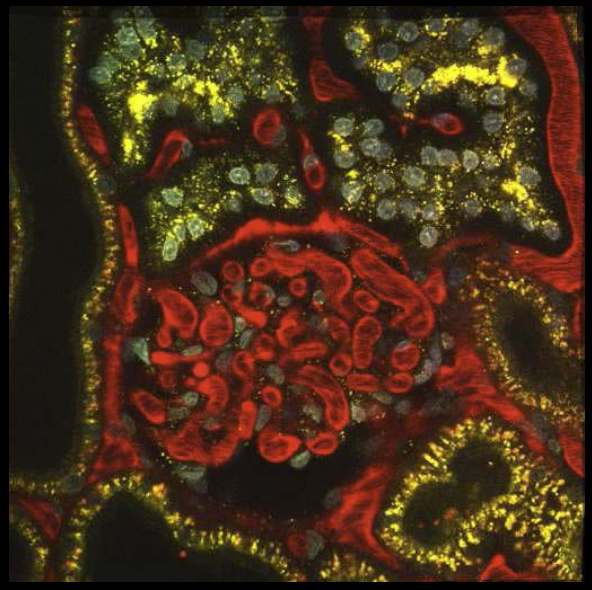


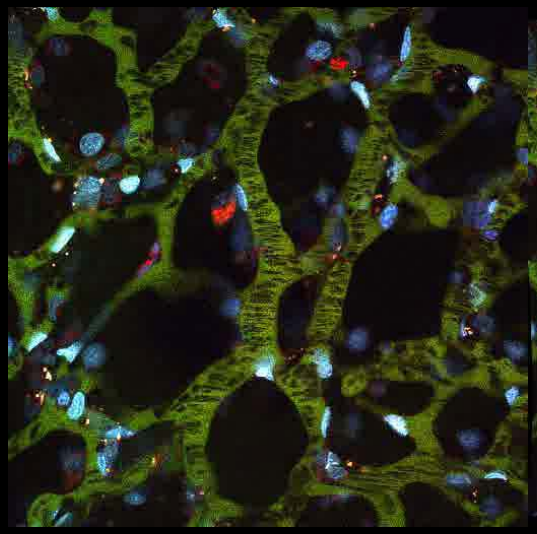
Reducing motion artifacts in intravital microscopy – Digital image registration

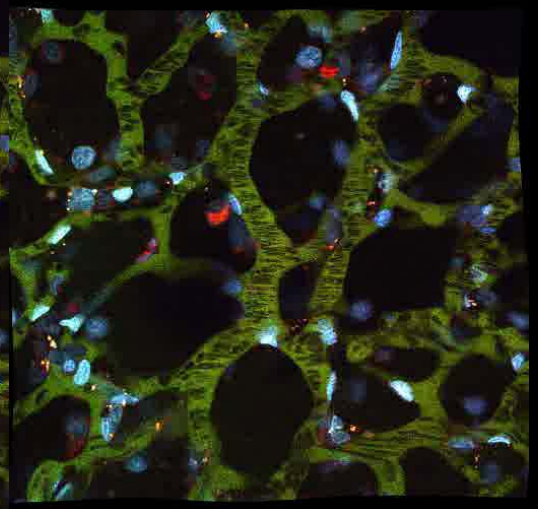
Before



After





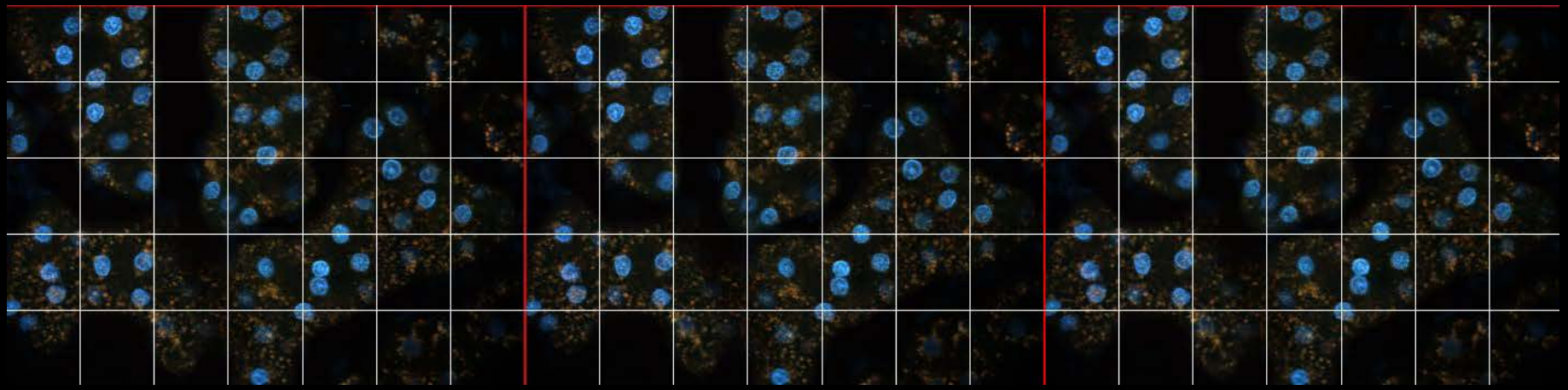


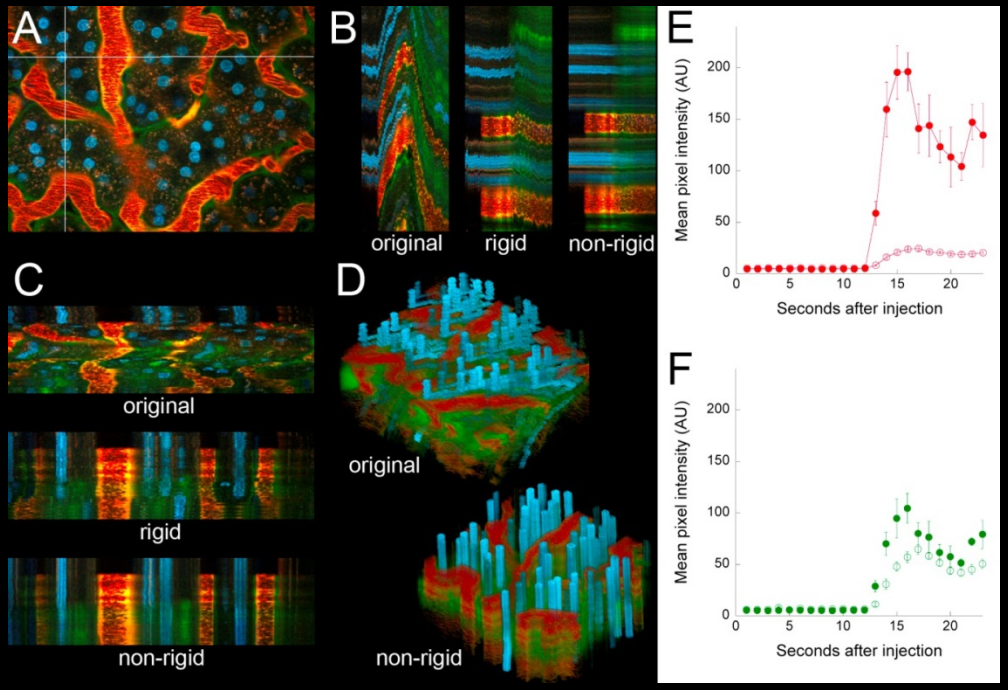
Before *After*

Presson, R., Brown, M., Sandoval, R., **Dunn, K.**, Lorenz, K., Delp, E., Salama, P., Molitoris, B. and Petrache, I. 2011. Two-photon imaging within the murine thorax without respiratory and cardiac motion artifact. Am. J. Path. 179:75-82

Lorenz, K.S., Salama, P., **Dunn, K.W.** and E.J. Delp. 2011. Non-rigid registration of multiphoton microscopy images using B-splines. Progress in Biomedical Imaging SPIE proceedings. 7962.

Reducing motion artifacts in intravital microscopy – Digital image registration





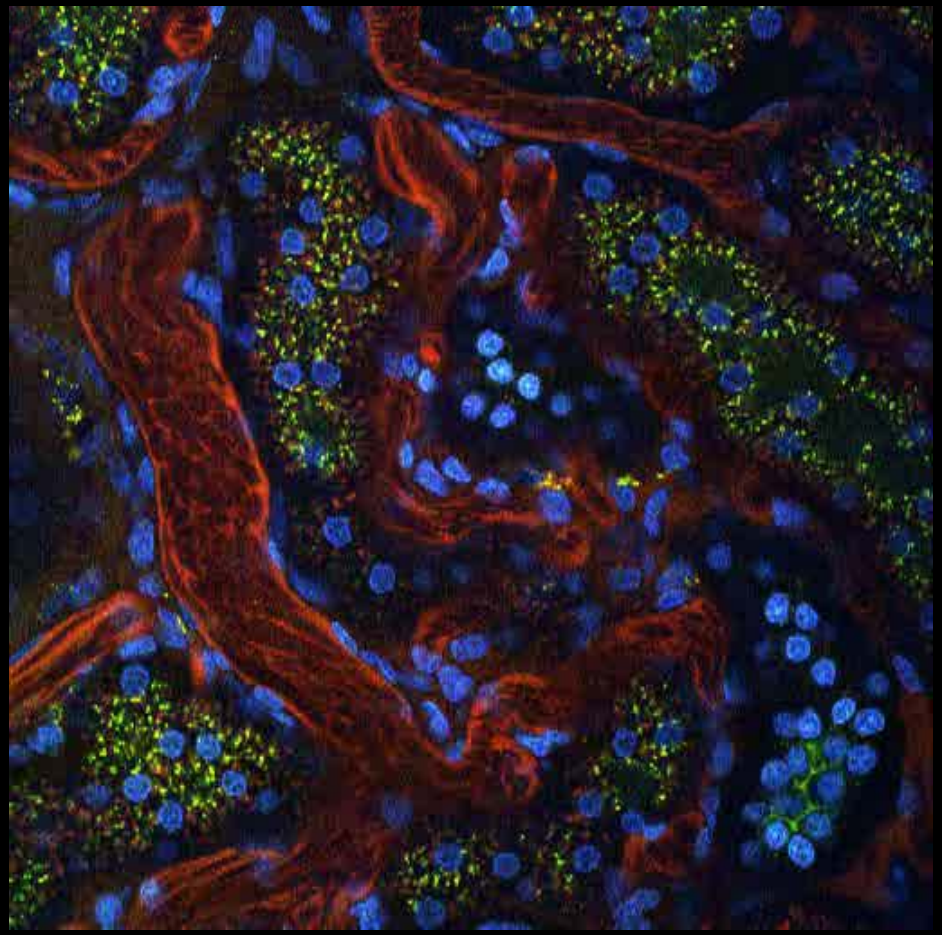
Dunn, Lorenz, Salama, and Delp. 2014. IMART software for correction of motion artifacts in images collected in intravital microscopy. Intravital. 3:e28210-1-10

Niraj Gadgil
Demo – Automated image analysis
Thursday afternoon

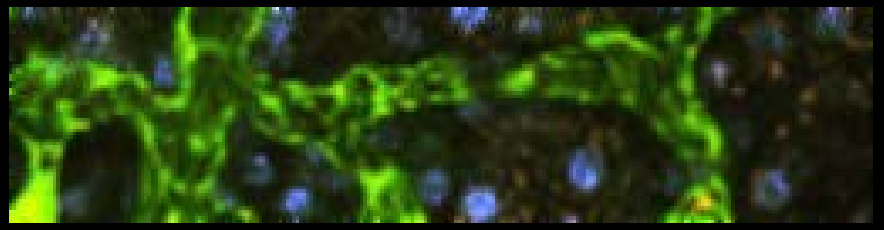
Challenges of subcellular imaging in living animals

- Motion artifacts from respiration and heartbeat
- Slow image capture rate

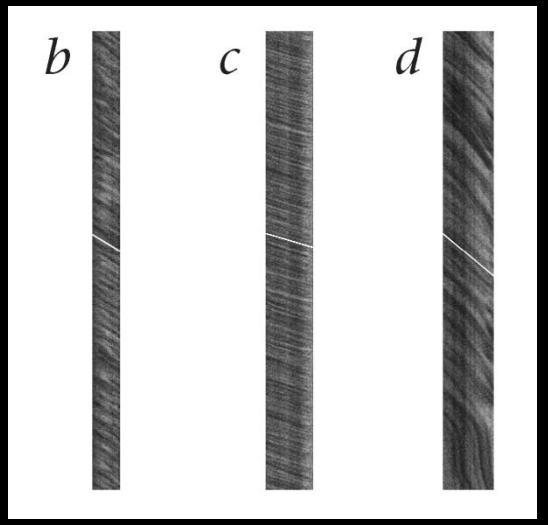
Single point scanning with a galvanometer
512 lines per second



One 512x512 frame per second



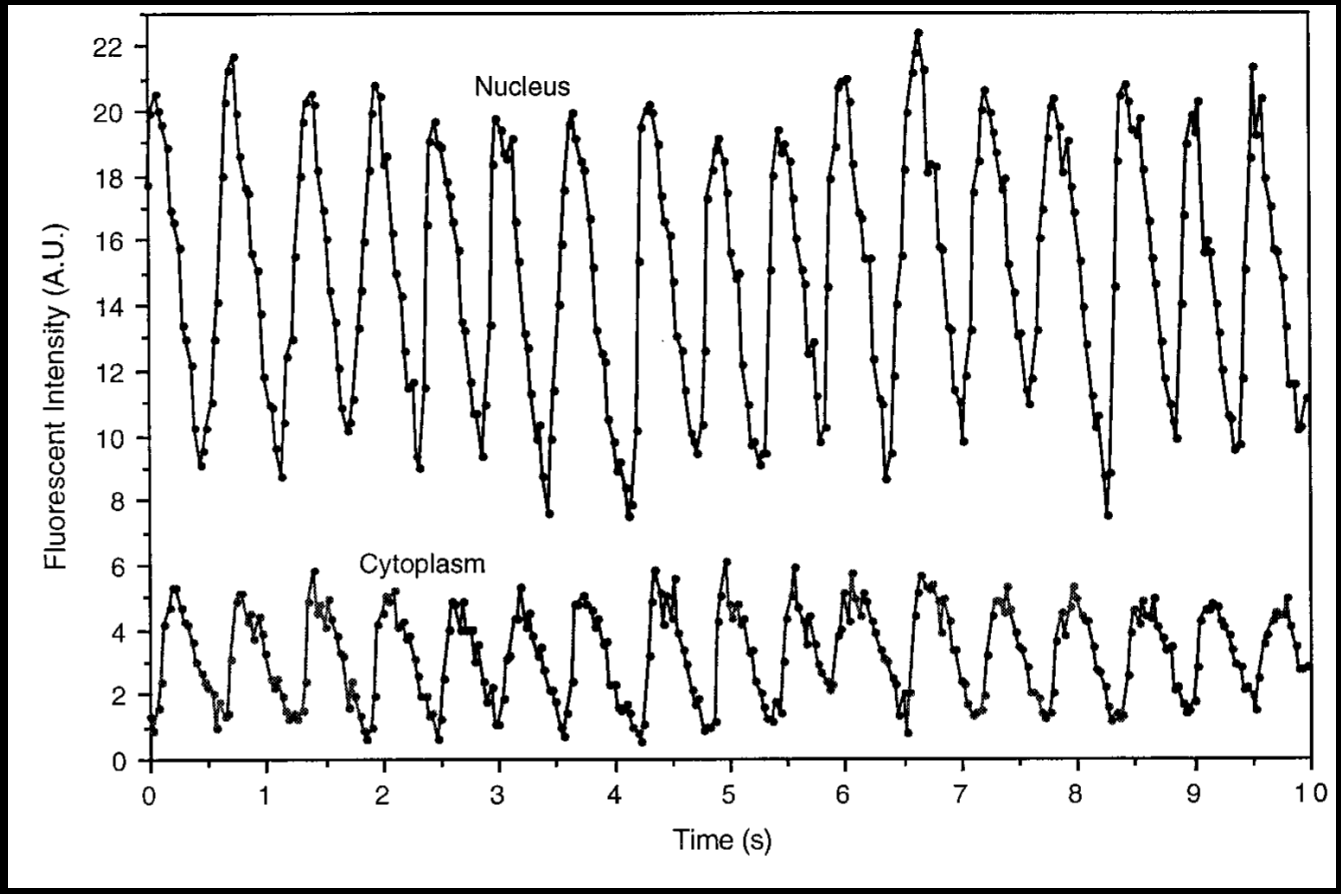
Four 512x128 frames per second



(Brown et al., 2001)

512 lines per second

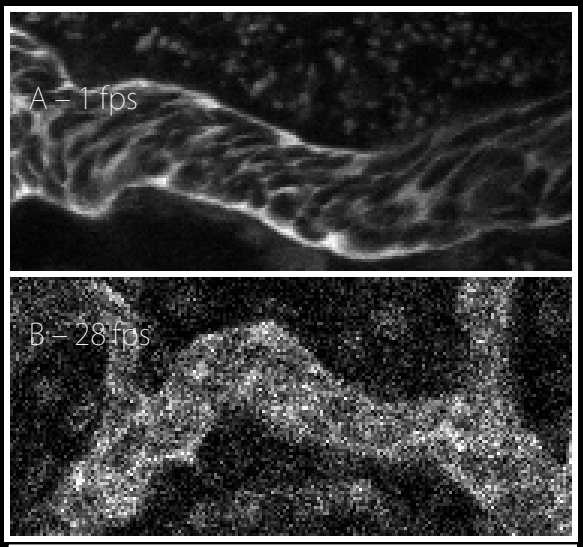
Single point scanning with a resonant scanner 15000 lines per second (30 fps)



Fan et al., 1999. Biophys. Journal 76:2412

Speed limits for multi-photon microscopy

30-fold higher frame rates require 30-fold shorter pixel dwell times which then requires 30 fold better signal. For most applications increasing the signal requires increasing the excitation.



Images of renal capillary of a living rat collected at 1 frame per second (A) or 28 fps (B).

- In many applications of multiphoton microscopy, power is already limiting – you may not be able to extract more signal with more power - 30 fold increase in signal requires 5.5 fold more power

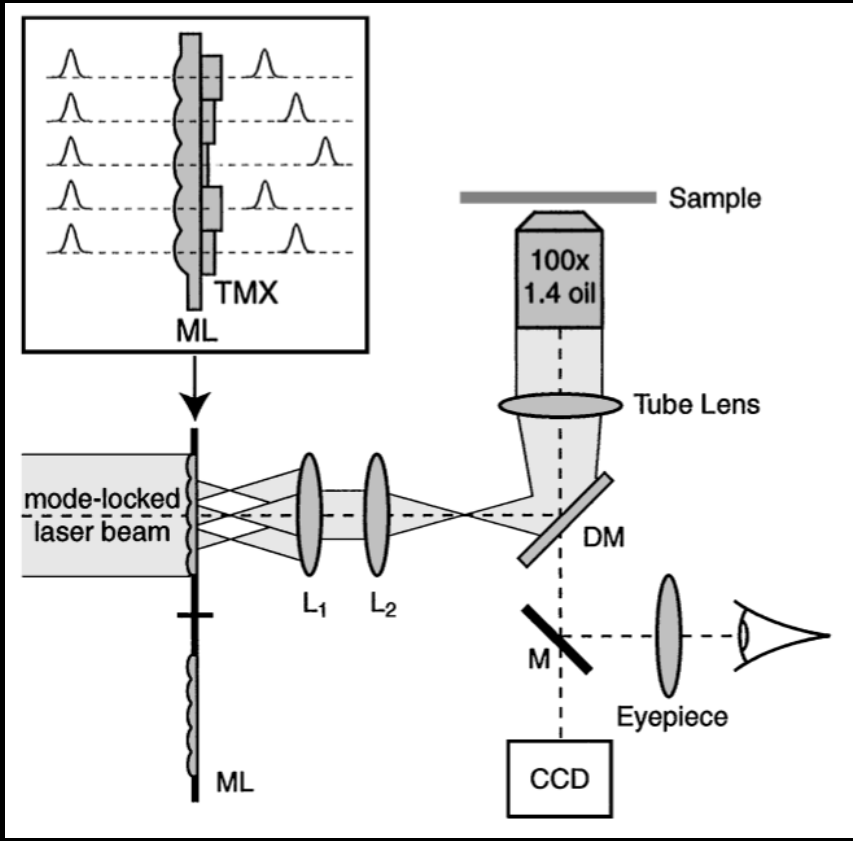
- In many applications, multiphoton imaging is done at power levels very close to fluorophore saturation – you may not get proportional increases in signal

- Photobleaching increases at greater than the cube of power – disproportionately more photobleaching than signal with more power

But, for experimental systems with sufficient fluorescence, resonant scanners are capable of capturing dynamics in vivo

Try the Leica SP8 MP system

Multi-point scanning multiphoton microscopy



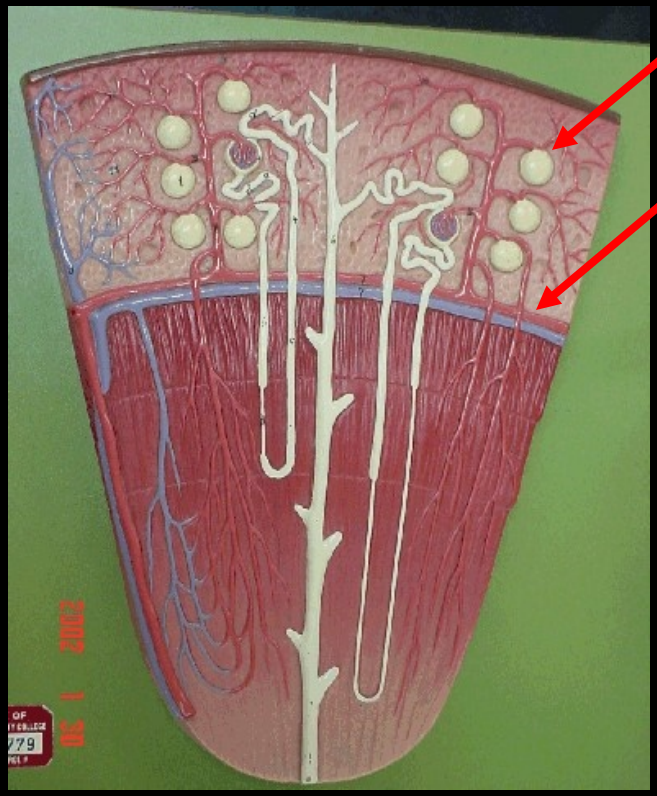
Andresen et al., 2001. Optics Letters 26:75

- Multi-focal systems speed image acquisition by parallel scanning
- Power is divided among multiple excitation points – laser power limits multiplexing
- Imaging onto a CCD results in scattered emissions being attributed to the wrong position in the image, increasing background and reducing resolution
- The system would thus be of limited utility for imaging deep into tissues, the conditions that justify multiphoton microscopy in the first place

Challenges of subcellular imaging in living animals

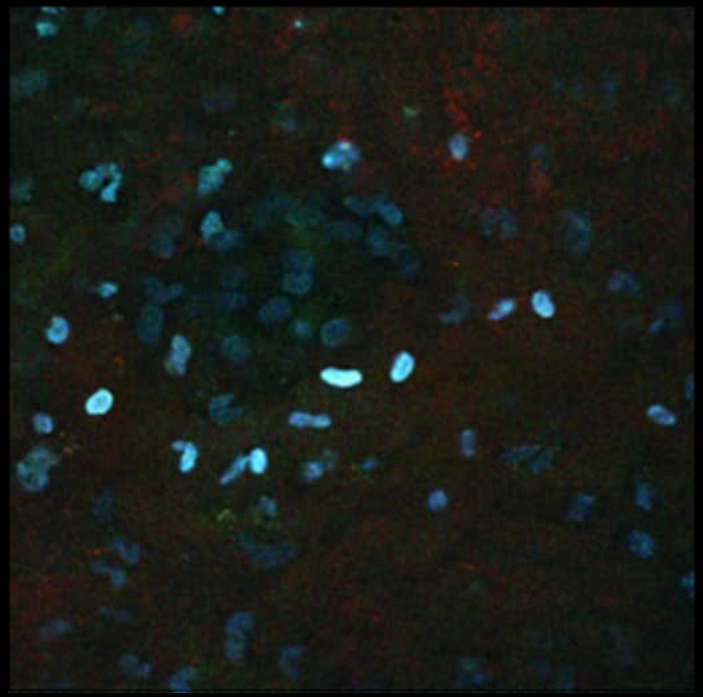
- Motion artifacts from respiration and heartbeat
- Slow image capture rate
- Limited reach/signal attenuation with depth

Multiphoton microscopy
Attenuation of signal with depth in the kidney



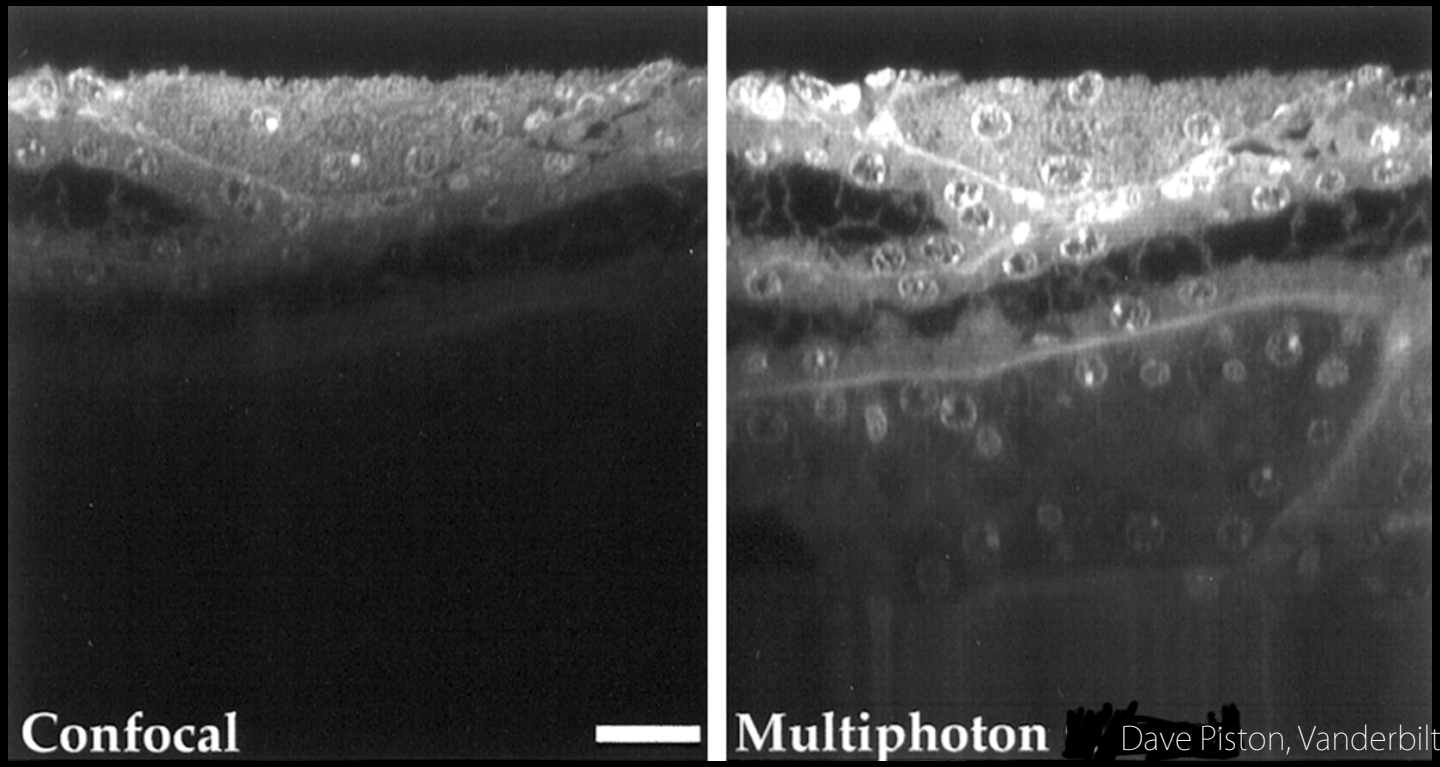
Glomeruli of most rats, mice are around 400 microns from the surface of the kidney

Cortico-medullary boundary is around 2 mm from the surface of the kidney



With a 60X NA 1.2 water immersion objective, signal attenuation prevents imaging deeper than around 100 microns in kidney of living rats

Multiphoton microscopy
Sources of signal attenuation of signal with depth



- Light absorption
- Light scattering
- Spherical aberration

Multiphoton microscopy
Light absorption as a source of signal attenuation with depth

Model light extinction as - $I_z = I_0 e^{-az}$

Where

I_z = intensity of light at depth z

a = the absorption coefficient

For fluorescence excitation

Near infrared light, $a = .05$ to $2\ cm^{-1}$ in biological tissues

So transmission attenuated by 50% in 0.35 - 14 cm

But excitation is proportional to I^2,

Excitation is attenuated by 75% in 0.35 - 14 cm

- Excitation reduced 75% in ~ 3500 to 140,000 microns - not a big deal

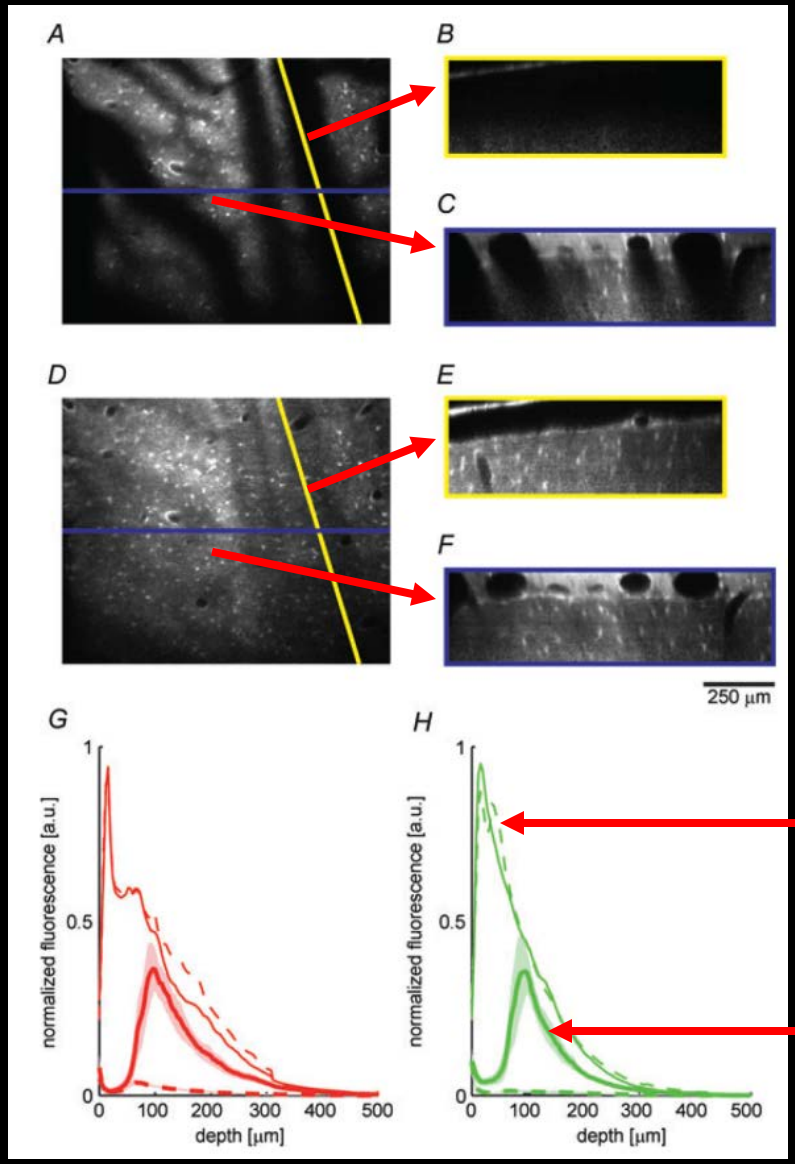
For collection of fluorescence emissions

For 550 nm light, $a = 4$ to $20\ cm^{-1}$ in biological tissues

- Transmission reduced 50% in 350-1730 microns – not a real big deal

Most investigators agree, absorption is seldom significant in biological tissues,
except in skin (melanin) and under blood vessels (hemoglobin)

Multiphoton microscopy
Absorption of light by blood (hemoglobin)



Blood perfusion

Perfluorocarbon perfusion

Change away from vessel

Change under vessel

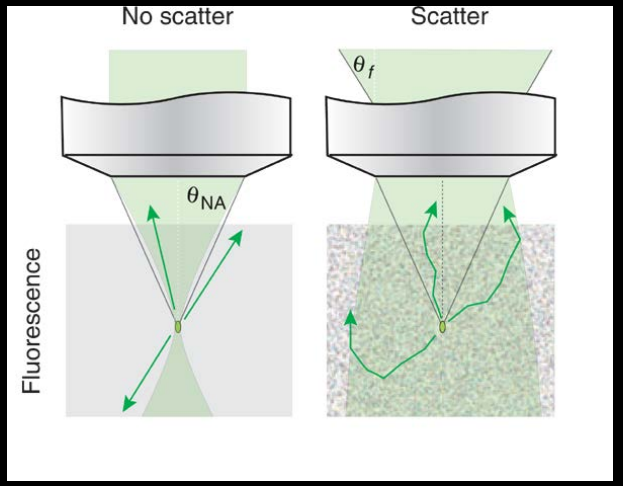
J Physiol 587.13 (2009) pp 3153–3158

Improved *in vivo* two-photon imaging after blood replacement by perfluorocarbon

F. Haiss[1], R. Jolivet[1], M. T. Wyss[1], J. Reichold[2], N. B. Braham[3], F. Scheffold[3], M. P. Krafft[4] and B. Weber[1]

[1]Institute of Pharmacology and Toxicology, University of Zurich, 8091 Zurich, Switzerland
[2]Institute of Fluid Dynamics, ETH Zurich, 8091 Zurich, Switzerland
[3]Department of Physics and Fribourg Center for Nanomaterials, University of Fribourg, 1700 Fribourg, Switzerland
[4]Université de Strasbourg, Institut Charles Sadron (CNRS), 23 rue du Loess, 67034 Strasbourg Cedex, France

Multiphoton microscopy
Light scattering as a source of signal attenuation with depth



Model light extinction as - $I_z = I_0 e^{-sz}$

Where

I_z = intensity of light at depth z
s = the scattering coefficient

For fluorescence excitation

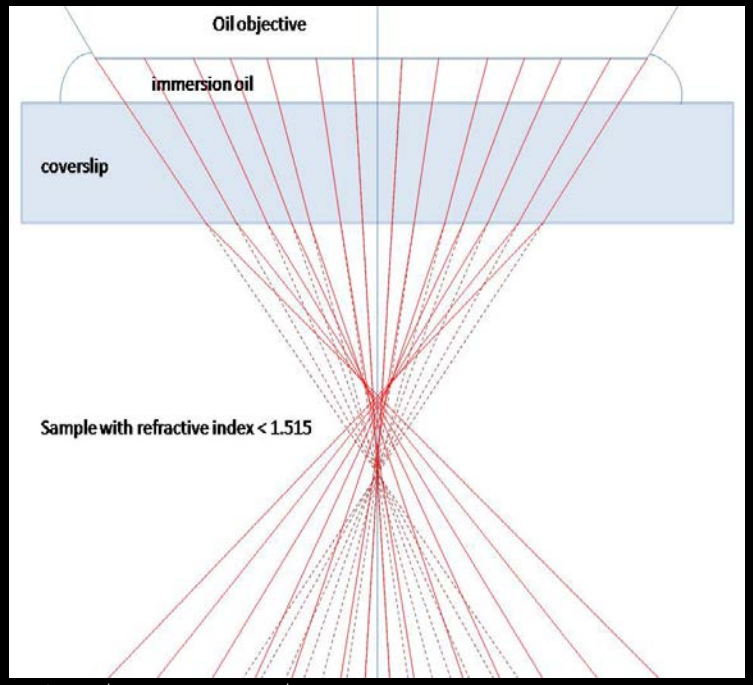
Near infrared light, s = 5 - 100 cm^{-1} in biological tissues
So transmission attenuated by 50% in 70 to 1400 microns
But excitation is proportional to I^2,
Excitation attenuated by 75% in 70 to 1400 microns

For collection of fluorescence emissions

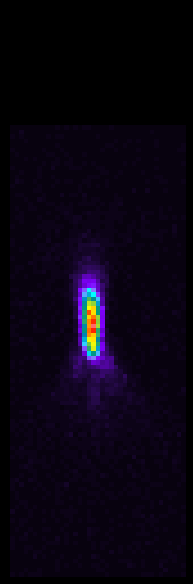
For 550 nm light, s = 100 – 500 cm^{-1} in biological tissues
So transmission attenuated by 50% in 15 - 70 microns
but even scattered emissions collected with non-descanned detectors

Multiphoton microscopy
Spherical aberration as a source of signal attenuation

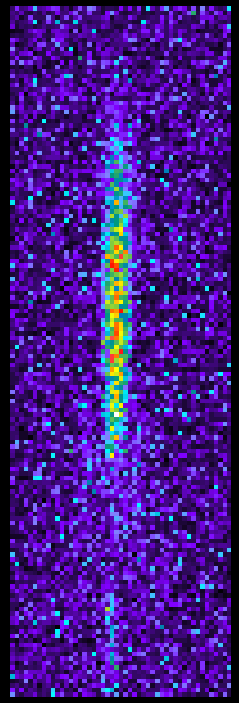
Two photon microscopy of fluorescent beads mounted in different media
using an oil-immersion objective



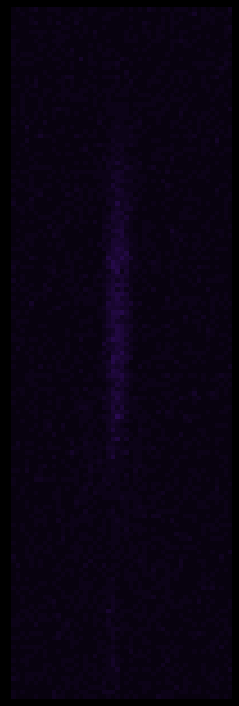
An oil-immersion objective imaging into an aqueous medium



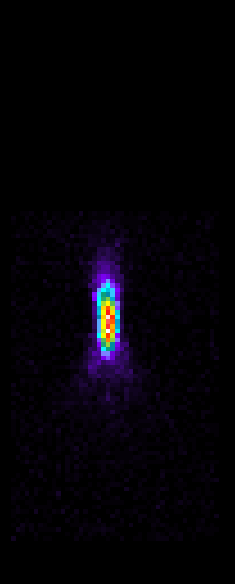
Surface
Aqueous



100um
Aqueous



100um
Aqueous
(w/out stretch)

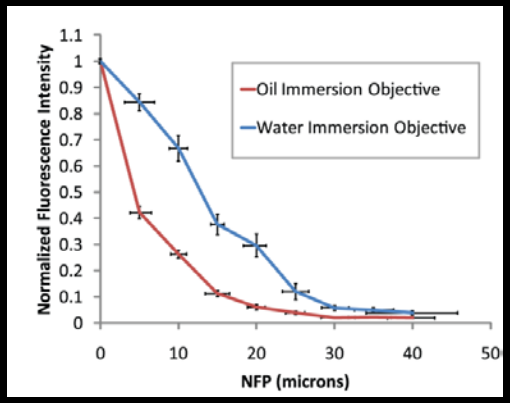


75um
1.5 RI medium

Since the average refractive index of the kidney is ~1.4, we incur spherical aberration with either water immersion or oil immersion objectives

Limited optical reach in the living kidney
Potential solutions

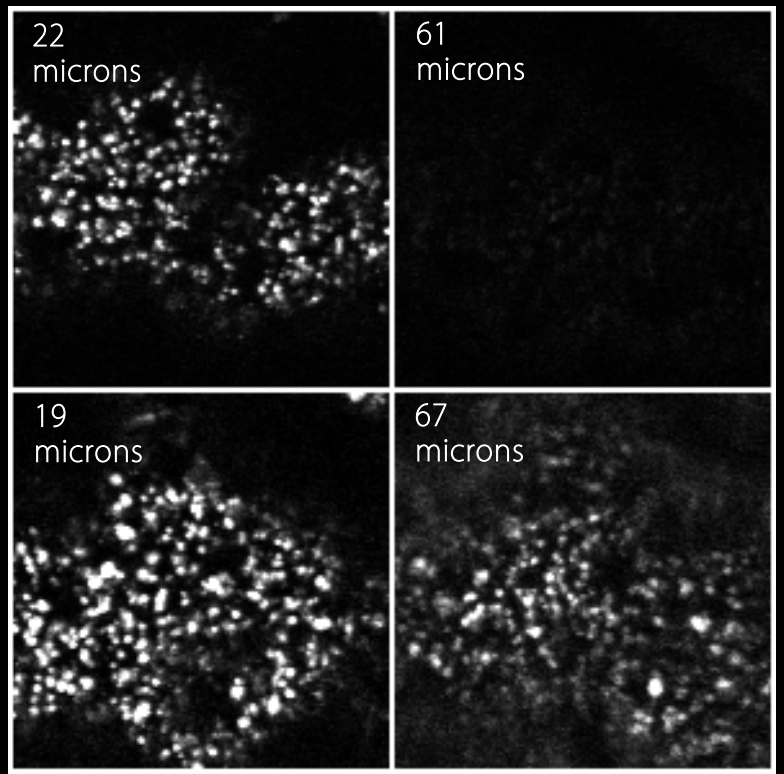
- Reduce optical aberrations



Young, Clendenon, Byars, Decca and Dunn. 2011. J. Microscopy

Olympus 25X, NA 1.05
Water immersion
objective
RI 1.33

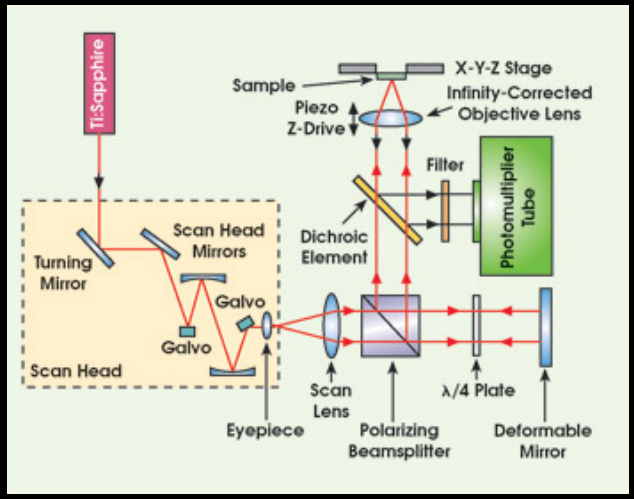
Olympus 30X, NA 1.05
Silicone oil immersion
objective
RI 1.4

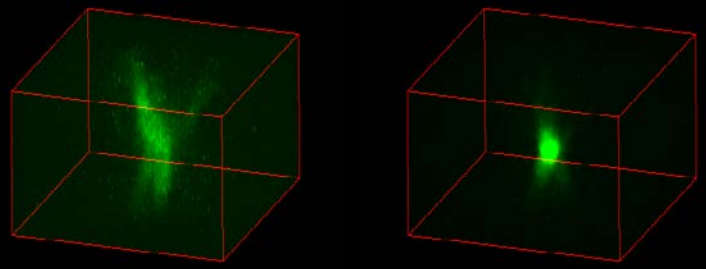


Limited optical reach in the living kidney
Potential solutions

- Reduce optical aberrations

Adaptive optics

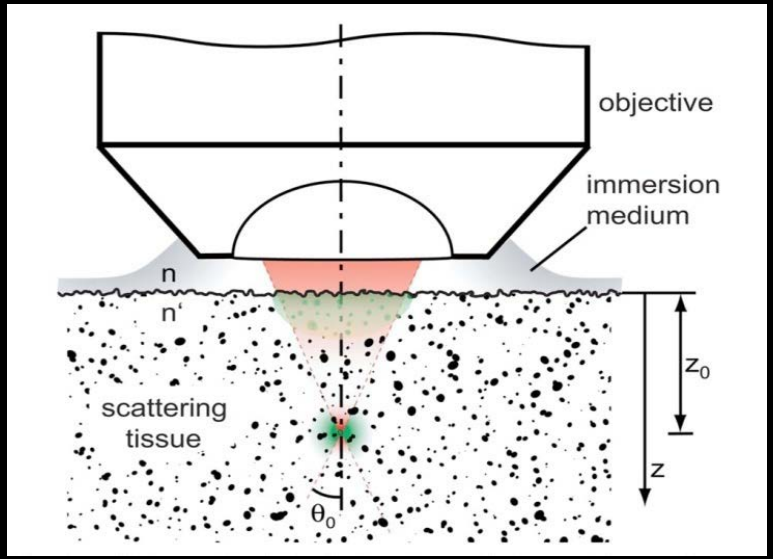




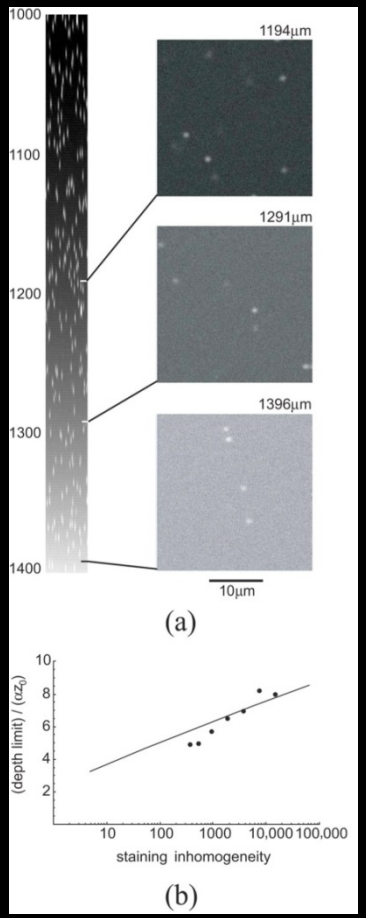
Confocal microscope images of 1 micron fluorescent spheres located below 100 microns of kidney tissue before (A) and after (B) adaptive optics correction – Joel Kubby, UCSC

Limited optical reach in the living kidney
Potential solutions

- Reduce optical aberrations
- Jack up the laser

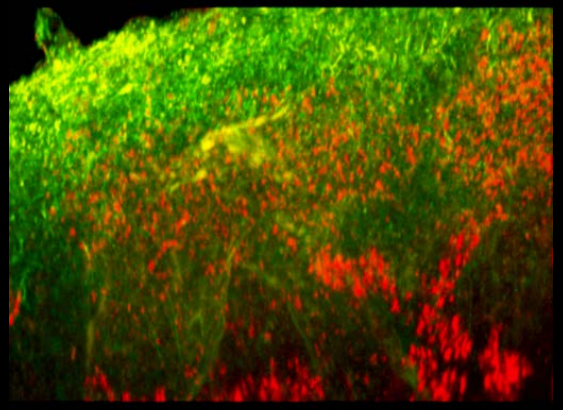


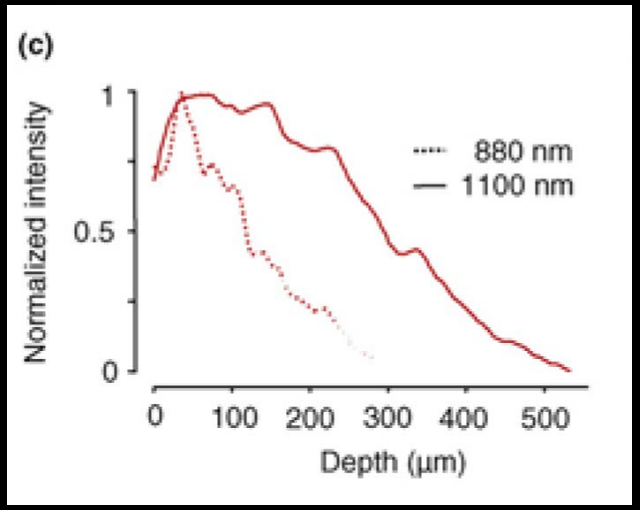
Imaging depth is ultimately limited by
near-surface fluorescence
- Theer and Denk, 2006



Limited optical reach in the living kidney
Potential solutions

- Reduce optical aberrations
- Jack up the laser
- Longer wavelengths of light

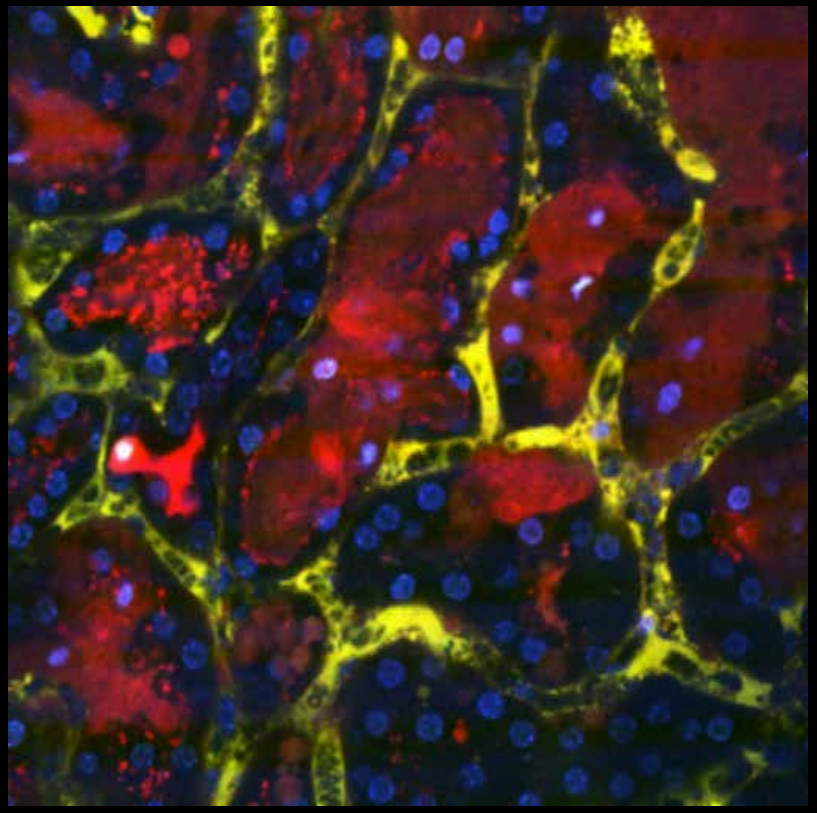




Andresen et al., 2009. Infrared multiphoton microscopy: subcellular-resolved deep tissue imaging. Curr. Opin. Biotech.

Limited optical reach in the living kidney
Potential solutions

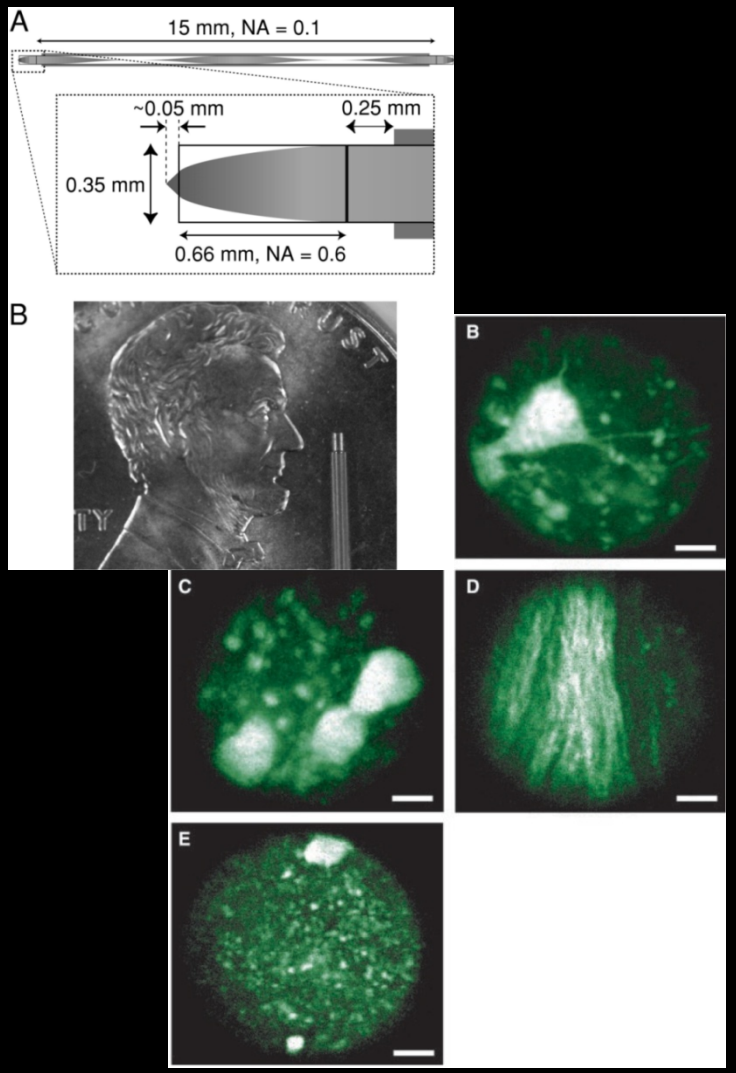
- Reduce optical aberrations
- Jack up the laser
- Longer wavelengths of light
- Invade the kidney - "cut down", GRIN lens, micro-prisms



Kidney “cut-down” or “parenchymal window”

Limited optical reach in the living kidney
Potential solutions

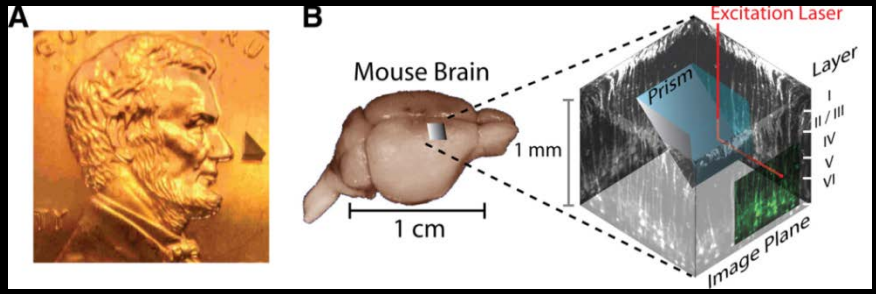
- Reduce optical aberrations
- Jack up the laser
- Longer wavelengths of light
- Invade the kidney - "cut down", GRIN lens, micro-prisms

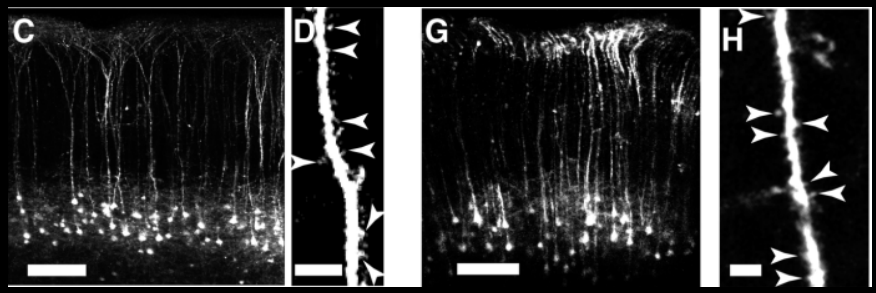


Gradient Index (GRIN) lens
Levene et al., 2004, J. Neurophysiol

Limited optical reach in the living kidney
Potential solutions

- Reduce optical aberrations
- Jack up the laser
- Longer wavelengths of light
- Invade the kidney - "cut down", GRIN lens, micro-prisms





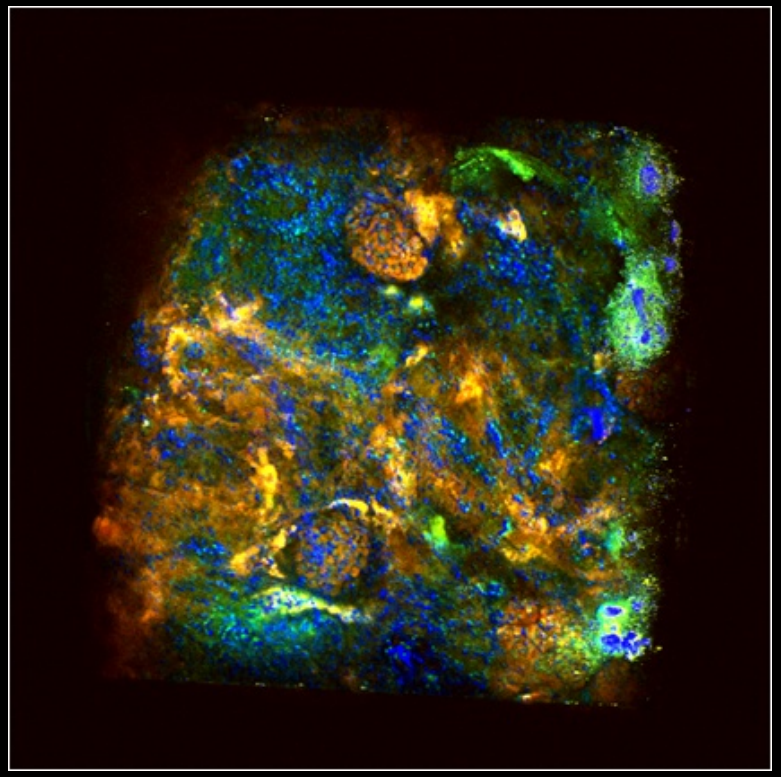
Conventional XY image in brain slice

XZ image in vivo with prism

Microprisms
Chia and Levene. 2009.

Limited optical reach in the living kidney
Potential solutions

- Reduce optical aberrations
- Jack up the laser
- Longer wavelengths of light
- Invade the kidney - "cut down", GRIN lens, micro-prisms



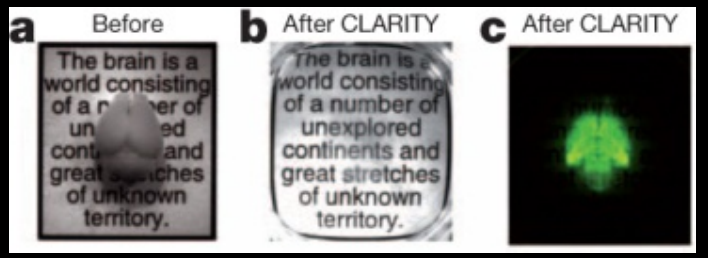
Microprisms
Gosia Kamocka and George Rhodes

Limited optical reach in the living kidney
Potential solutions

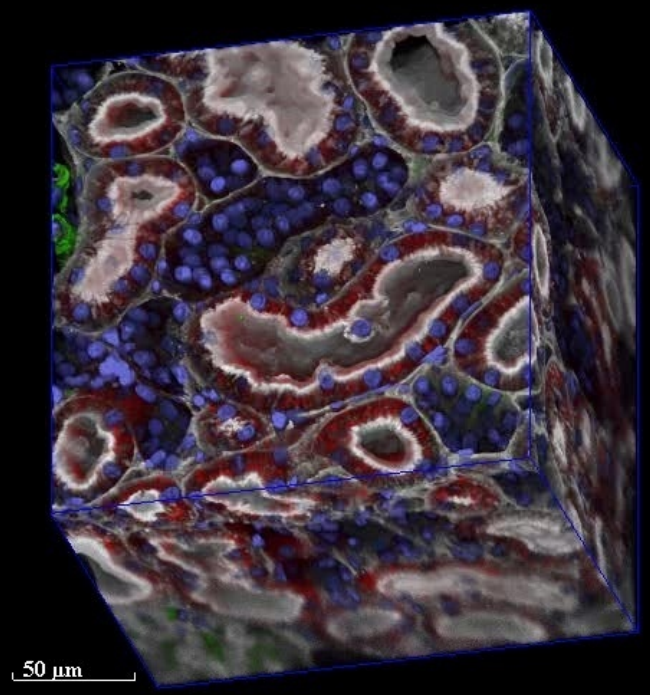
- Reduce optical aberrations
- Jack up the laser
- Longer wavelengths of light
- Invade the kidney - "cut down", GRIN lens, micro-prisms
- Reduce scattering – give up IVM

Kris Fertig, Leica
Demo – 3D imaging of cleared tissue
Wednesday, Thursday afternoon

Jeff Clendenon
3D Image visualization and analysis
Wedat 10:20am, Demo Wed afternoon



Chung et al., 2003



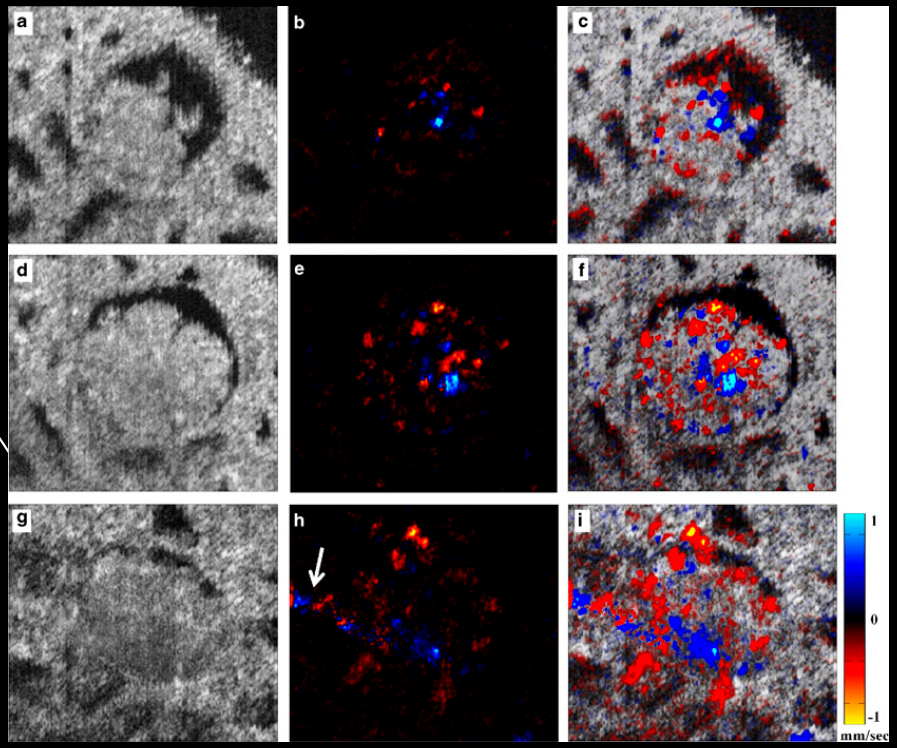
Tissue clearing

Clendenon, Ferkowicz, Young, and Dunn. 2011. Deep Tissue Fluorescent Imaging in Scattering Specimens Using Confocal Microscopy. Microscopy and Microanalysis.

Limited optical reach in the living kidney
Potential solutions

- Reduce optical aberrations
- Jack up the laser
- Longer wavelengths of light
- Invade the kidney - "cut down", GRIN lens, micro-prisms
- Reduce scattering – give up IVM
- Optical coherence tomography

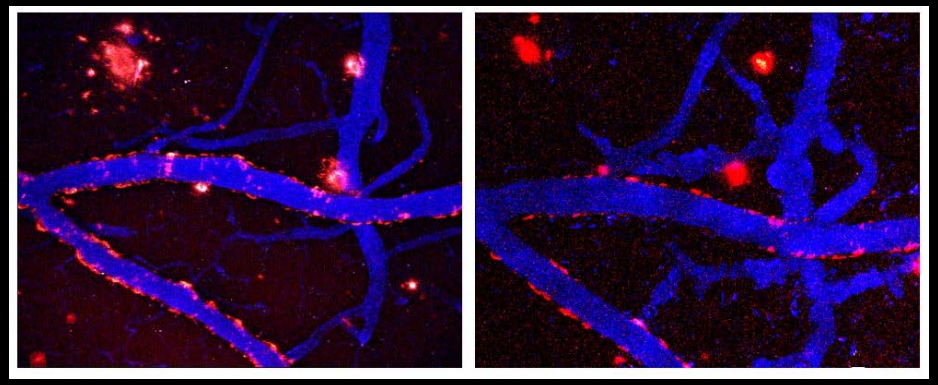
Yu Chen
OCT of the kidney
Wednesday at 9:20 am
Demos Wed and Thurs afternoons



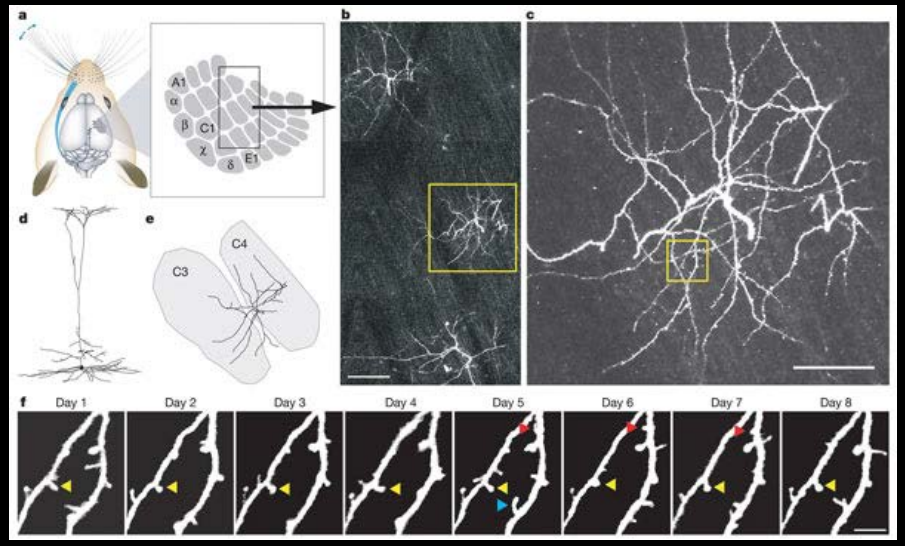
Combined Optical Coherence Tomography (left) and Doppler Optical Coherence Tomography (middle) of living rat glomerulus

Wierwille, Andrews, Onozato, Jiang, Cable and Chen, 2011

Quantitative intravital microscopy circumventing the effects of depth on signal levels



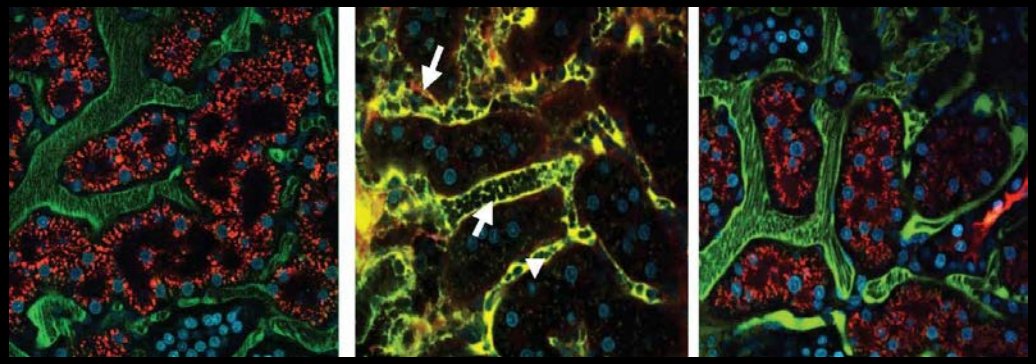
Amyloid plaque dynamics - Brian Bacskai, Harvard



Dendritic spine dynamics - Karel Svoboda, Janelia Farm

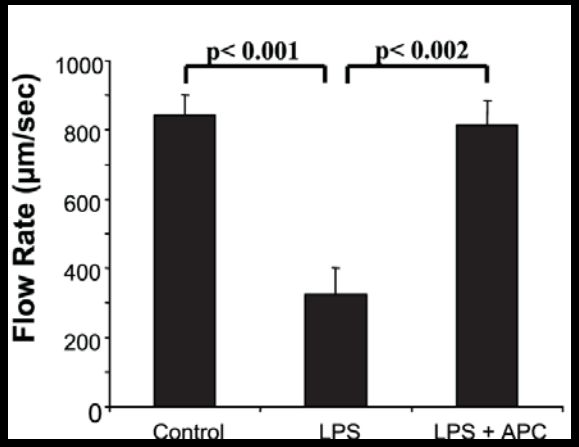
- Quantify without intensity
  –Structural changes

Quantitative intravital microscopy circumventing the effects of depth on signal levels



Sham LPS LPS + APC

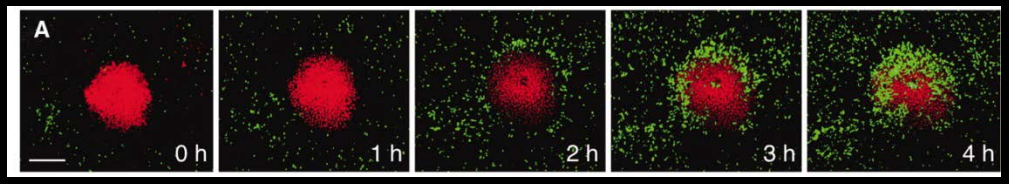
- Quantify without intensity
  - –Structural changes
  - –Motion

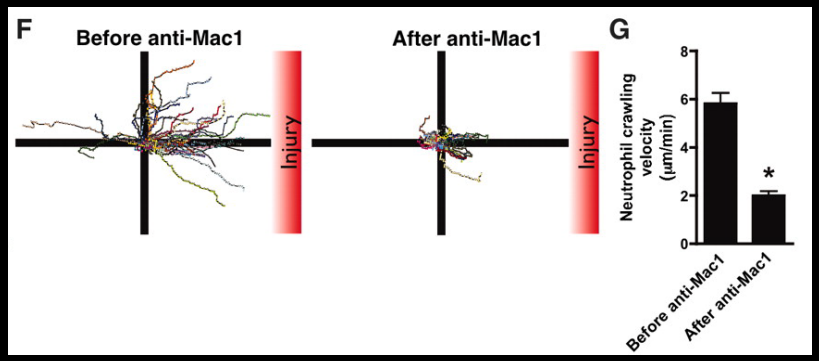


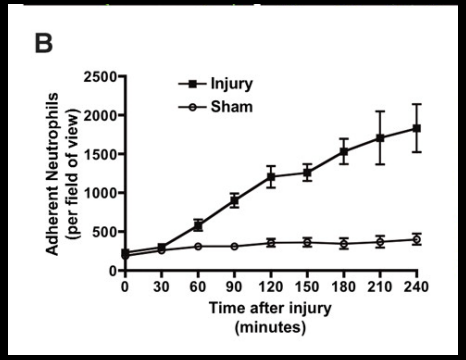
Microvascular flow

Sharfuddin Sandoval, Berg, McDougal, Campos, Phillips, Jones, Gupta, Grinnell and Molitoris. 2009. Soluble thrombomodulin protects ischemic kidneys. J Am Soc Nephrol:524-34.

Quantitative intravital microscopy circumventing the effects of depth on signal levels



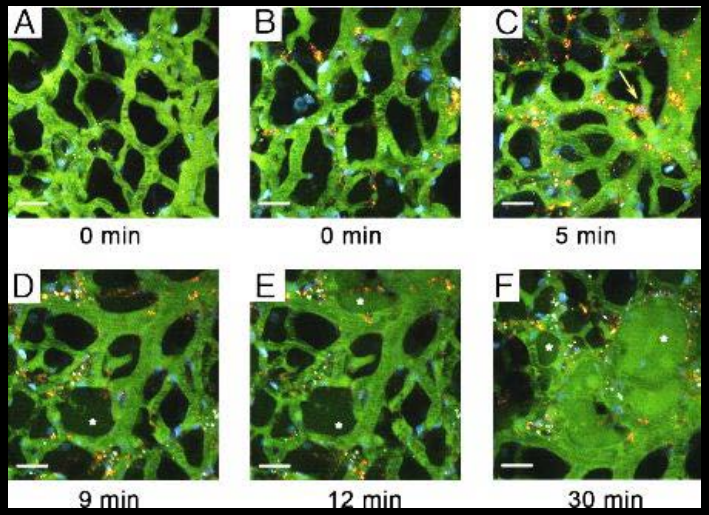




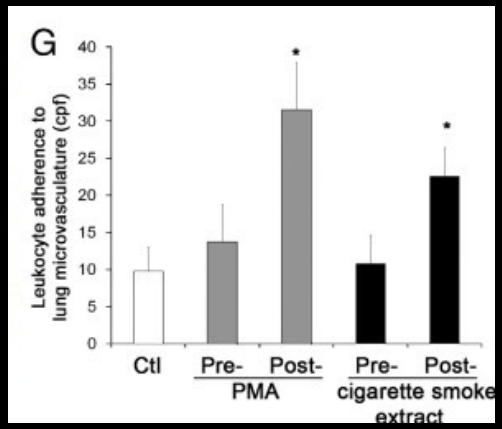
Neutrophil migration – Paul Kubes, Calgary

- Quantify without intensity
  - –Structural changes
  - –Motion
  - –Incidence

Quantitative intravital microscopy circumventing the effects of depth on signal levels



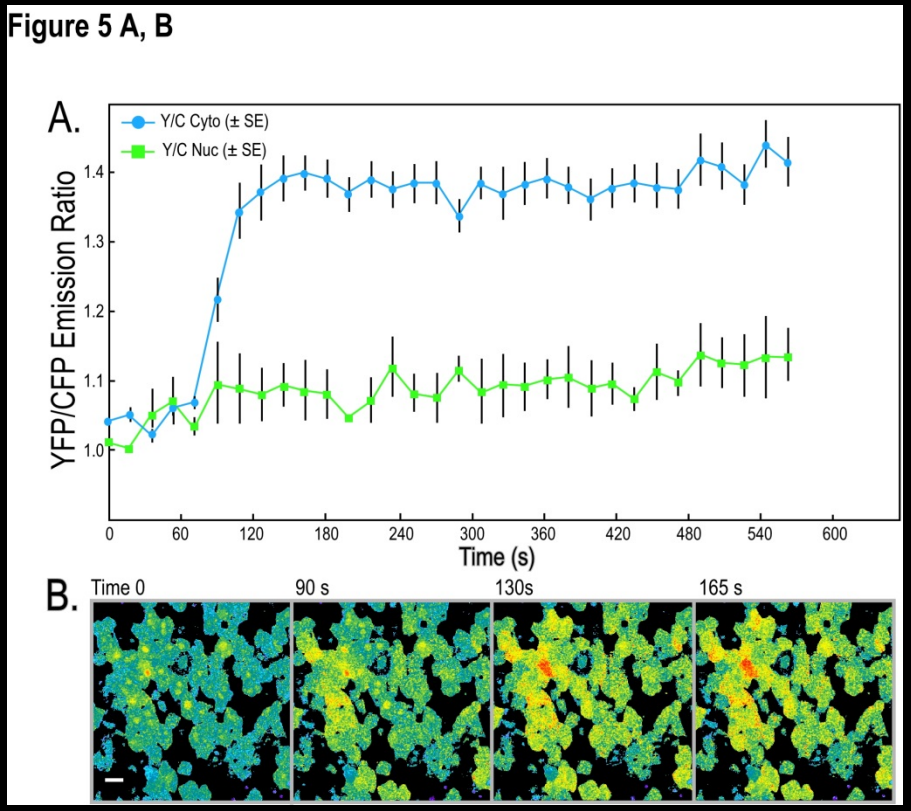
- Quantify without intensity
  - –Structural changes
  - –Motion
  - –Incidence



White cell recruitment

R.G. Presson Jr., M.B. Brown, A.J. Fisher, R.M. Sandoval, K.W. Dunn, K.S. Lorenz, E.J. Delp, P. Salama, B.A. Molitoris, I. Petrache, 2011. *Ameri. J. Path*, 179, :75-82

Quantitative intravital microscopy circumventing the effects of depth on signal levels



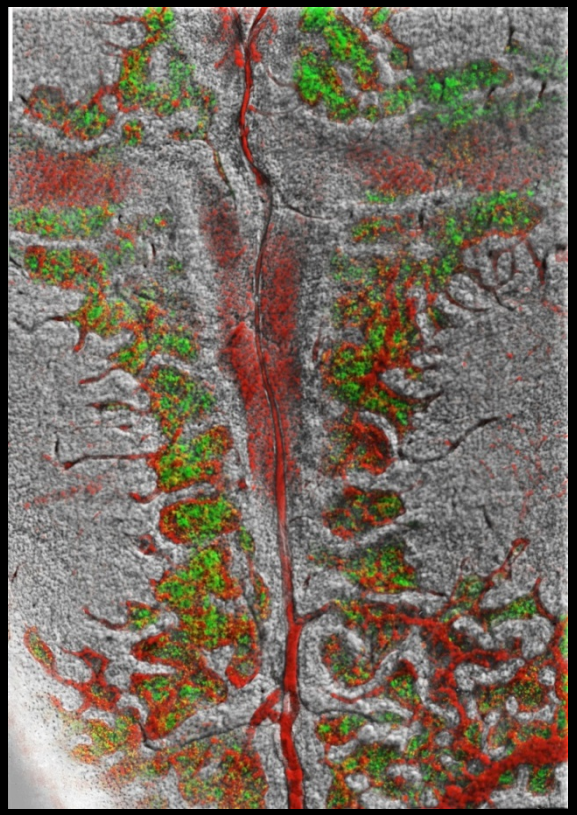
PKA activation in mouse liver– AKAR4.1 FRET sensor

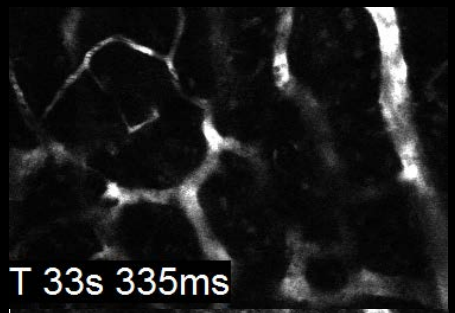
Practical method for monitoring FRET-base biosensor probe activities using two-photon excitation microscopy
Tao et al., in prep

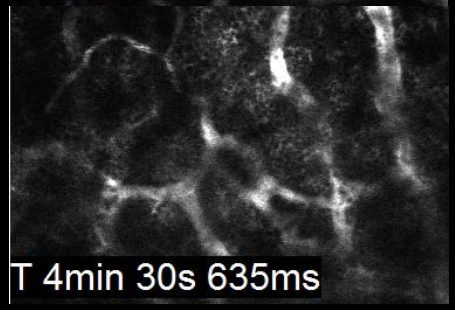
- Quantify without intensity
  - –Structural changes
  - –Motion
  - –Incidence
- Quantify relative intensities
  - –Ratiometric measures

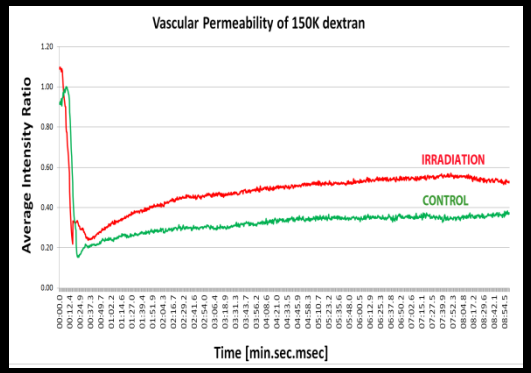
Richard Day
Fluorescent proteins – Tomorrow at 10:20
FRET – Wednesday Lunch
Fluorescence lifetime microscopy demo – Wed PM

Quantitative intravital microscopy circumventing the effects of depth on signal levels







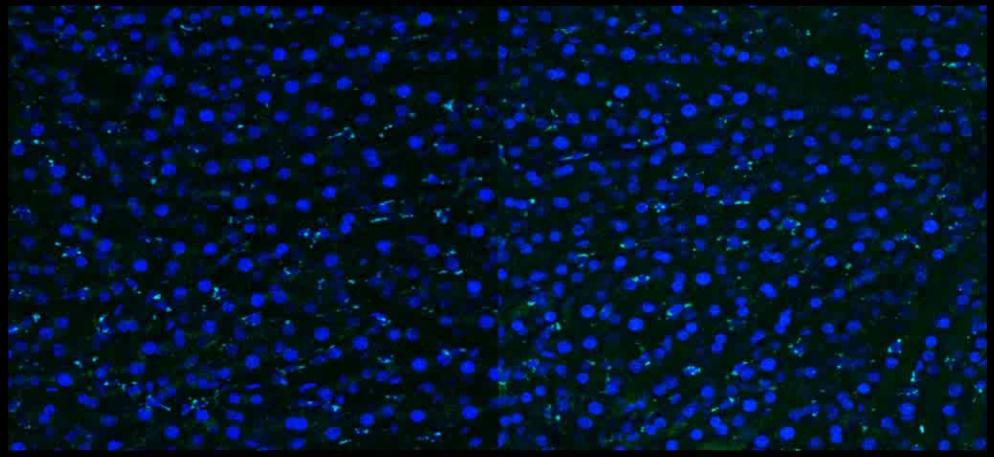


- Quantify without intensity
  - –Structural changes
  - –Motion
  - –Incidence
- Quantify relative intensities
  - –Ratiometric measures

Microvascular leakage in the bone marrow space of the mouse calvarium

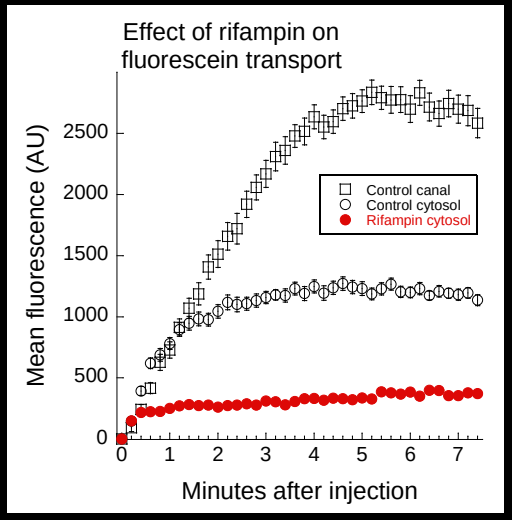
Malgorzata Kamocka, Amy Zollman and Nadia Carlesso - IUSM

Quantitative intravital microscopy circumventing the effects of depth on signal levels



Vehicle treated

Rifampin treated



- Quantify without intensity
  - –Structural changes
  - –Motion
  - –Incidence
- Quantify relative intensities
  - –Ratiometric measures
  - –Time-series measures

Seth Winfree
Demonstration – Quantitative image analysis
Monday, Tuesday afternoon

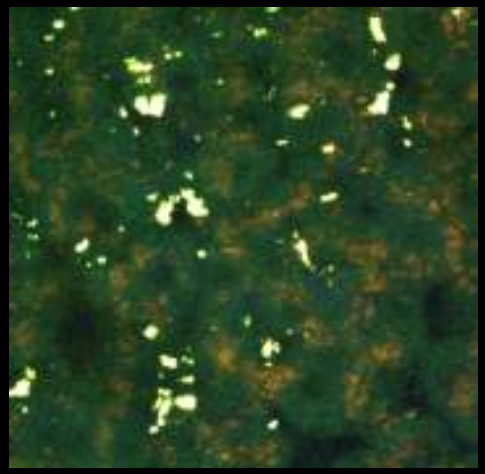
Babbey et al., 2012. Quantitative intravital microscopy of hepatic transport. Intravital. 1:44-53

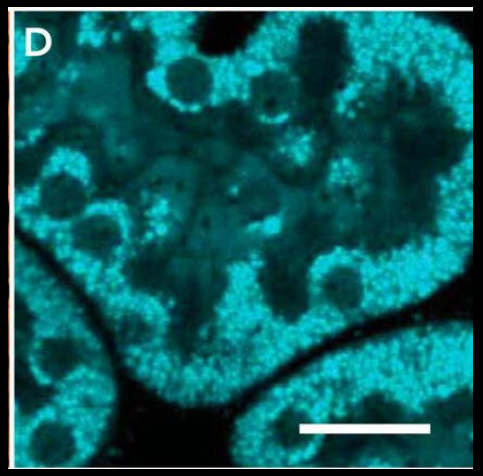
Challenges of subcellular imaging in living animals

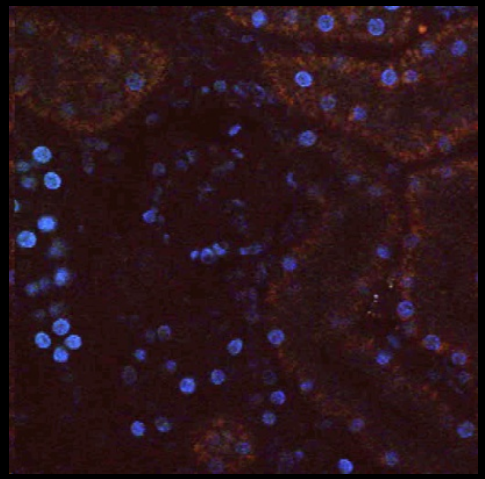
- Motion artifacts from respiration and heartbeat
- Slow image capture rate
- Limited reach/signal attenuation with depth
- In vivo labeling

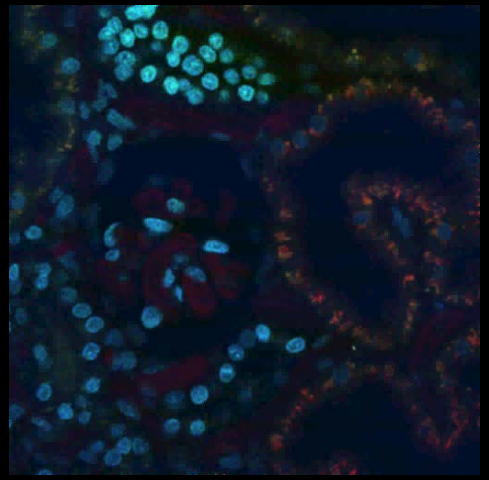
Sources of contrast in intravital multiphoton microscopy

- Autofluorescence
- Hoechst 33342
- Intravenous bulk probes







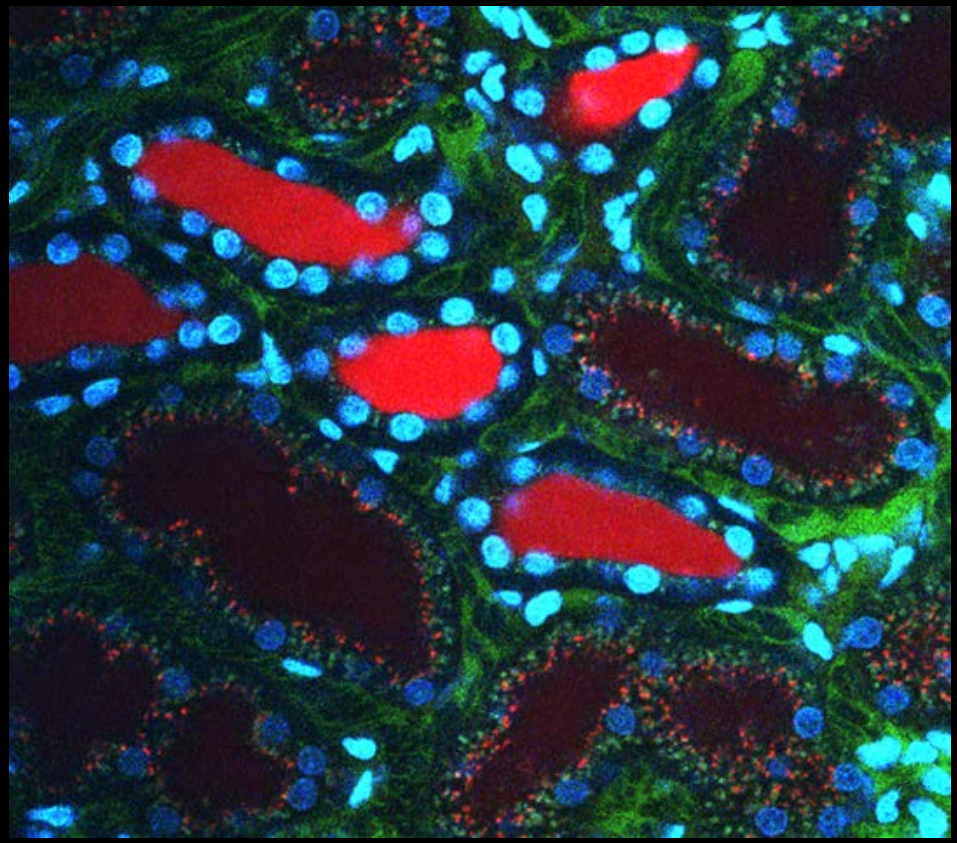


Ruben Sandoval
Silvia Campos-Bilderback
Demonstration – Glomerular filtration
Monday, Tuesday afternoon

Intravital microscopy of multiple kidney functions via intravenous injection of fluorescent probes

Simultaneous imaging of a rat injected with fluorescent dextrans and Hoechst 33342 reveals multiple processes

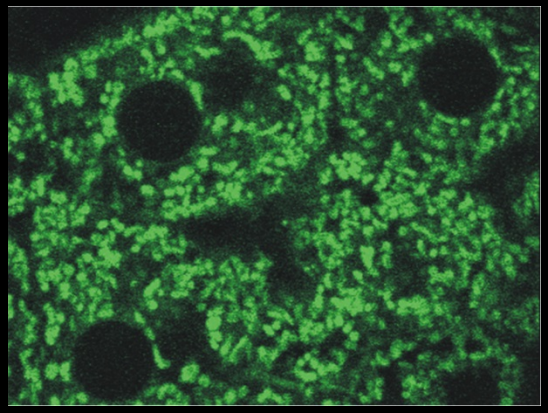
- glomerular filtration
- proximal tubule endocytosis
- tubular solute concentration
- tubular flow
- capillary blood flow
- vascular permeability
- apoptosis
- tubular sloughing



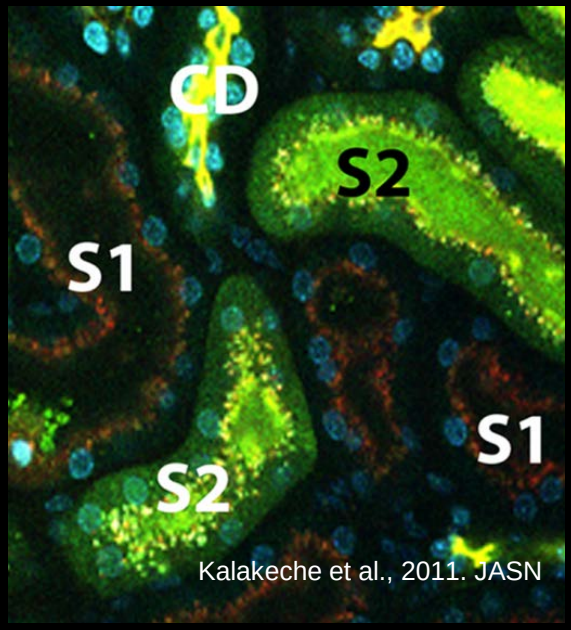
Dunn et al., 2002. AJP Cell. 283:C905-C916

Sources of contrast in intravital multiphoton microscopy

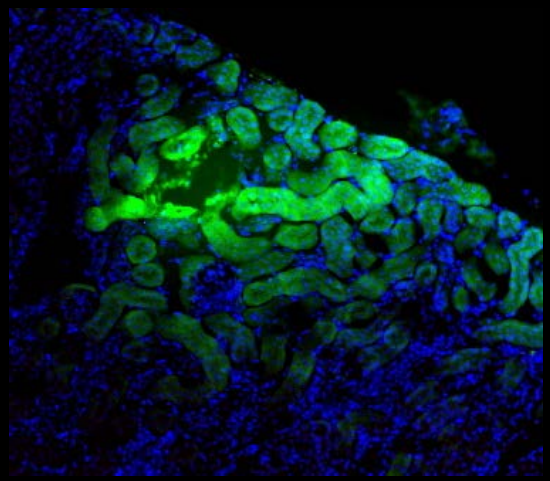
- Autofluorescence
- Hoechst 33342
- Intravenous bulk probes
- Permeant bio-indicators



Rhodamine 123 in liver mitochondria –
John Lemasters



DCFDA labeling S2 cells in oxidative stress
Pierre Dagher

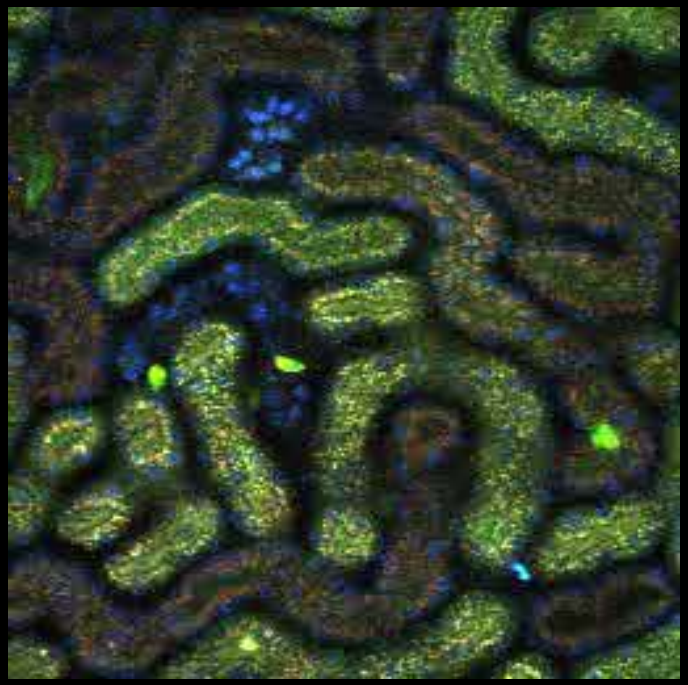


CMFDA delivered to cytosol by
subcapsular injection
Rudy Juliano, UNC

Pierre Dagher
Fluorescent probes for studying AKI
Tomorrow at 11:10 AM

Gosia Kamocka
George Rhodes
Demo – Mitochondria, Oxid. stress
Monday, Tuesday afternoon

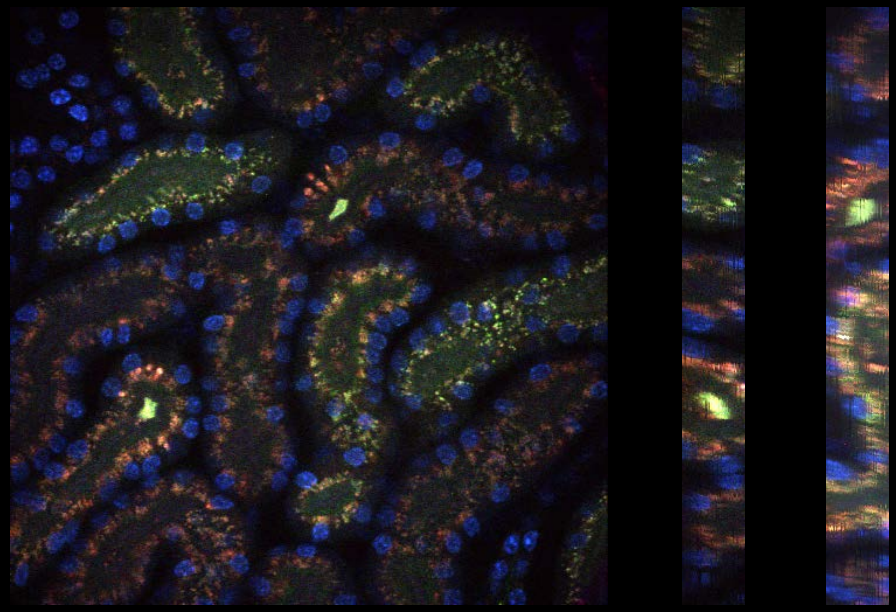
In vivo labeling of renal macrophages

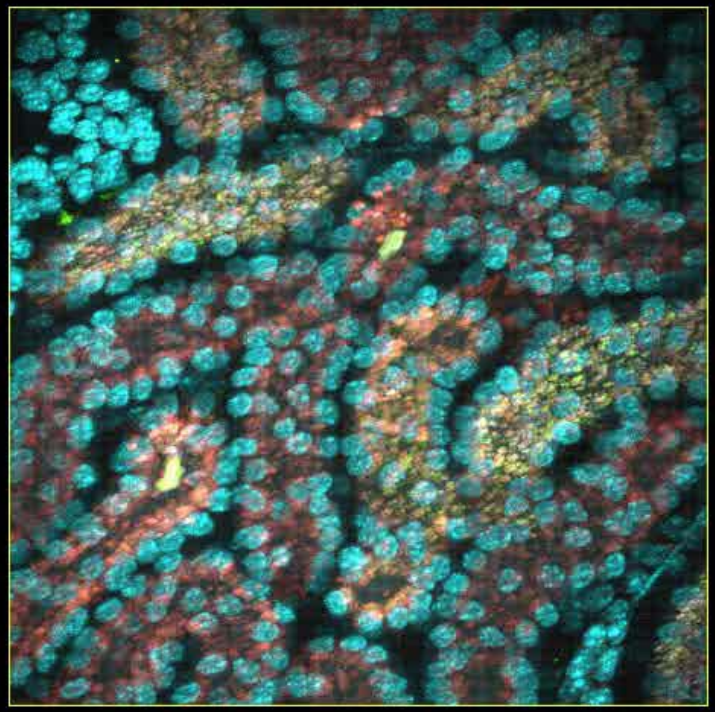


Calcein loaded into macrophages by phagocytosis of
pH-sensitive liposomes containing calcein
Takashi Hato and Pierre Dagher
(30x)

Calcein-loaded pH-sensitive liposomes provided by
Rudy Juliano, UNC

In vivo labeling of renal macrophages



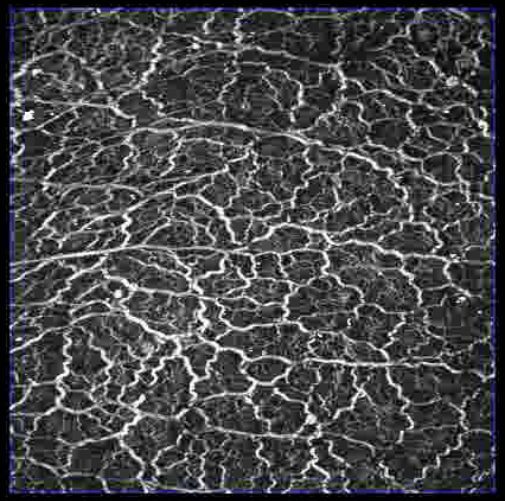


Calcein loaded into macrophages by phagocytosis of pH-sensitive liposomes containing calcein
Takashi Hato and Pierre Dagher
(30x)

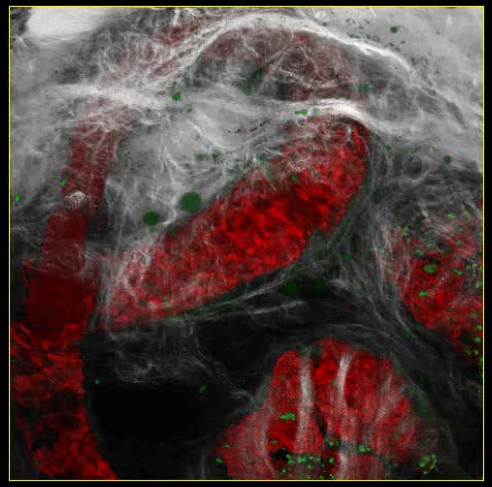
Calcein-loaded pH-sensitive liposomes provided by
Rudy Juliano, UNC

Sources of contrast in intravital multiphoton microscopy

- Autofluorescence
- Hoechst 33342
- Intravenous bulk probes
- Permeant bio-indicators
- Second harmonic generation



Liver of living mouse
Gosia Kamocka and Amy Zollman



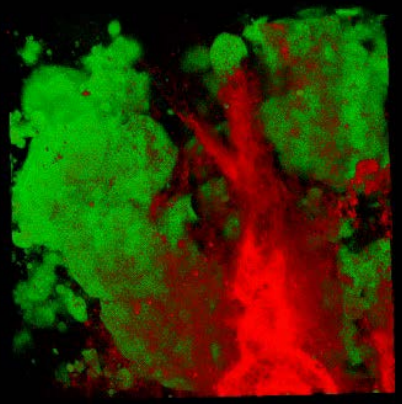
Ex vivo human sweat gland
Mary Beth Brown

Xinde Li
Label-free optical imaging
Thursday at 11:10

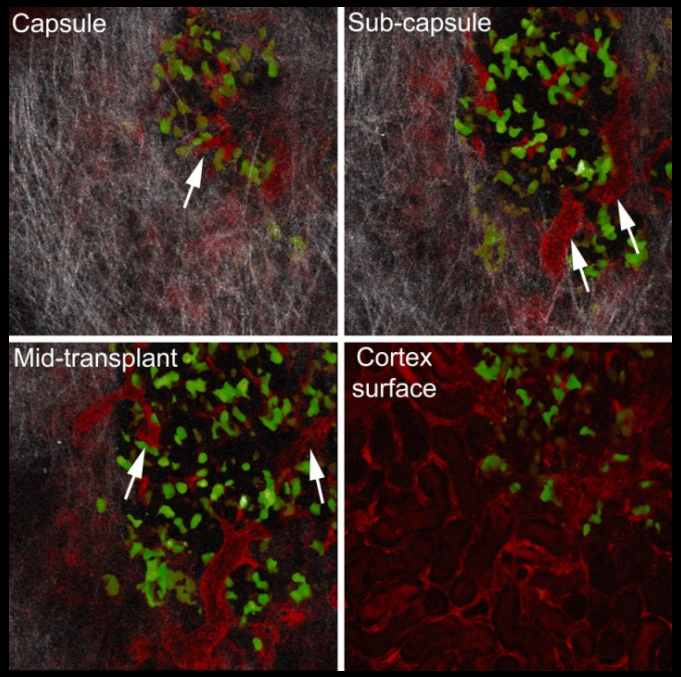
Sources of contrast in intravital multiphoton microscopy

- Autofluorescence
- Hoechst 33342
- Intravenous bulk probes
- Permeant bio-indicators
- Second harmonic generation
- Adoptive transfer

Henry Mang
Demonstration –IVM of mouse kidney
Monday, Tuesday afternoon



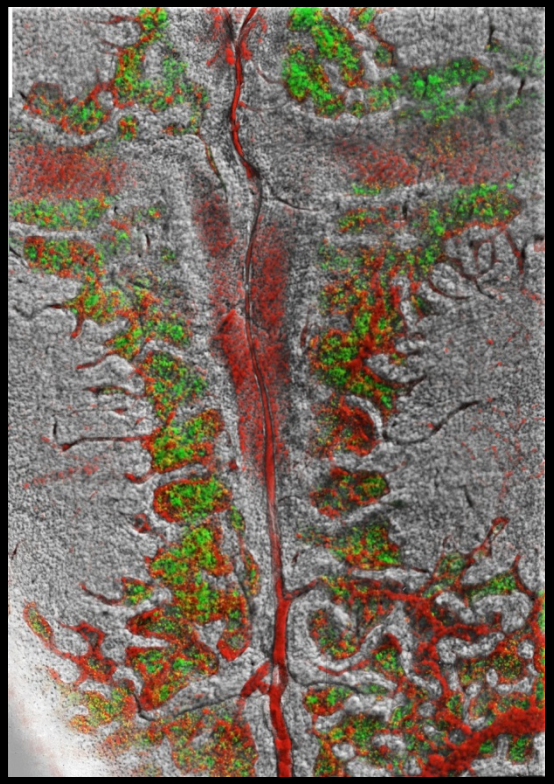
Prostate tumor
Tom Gardner



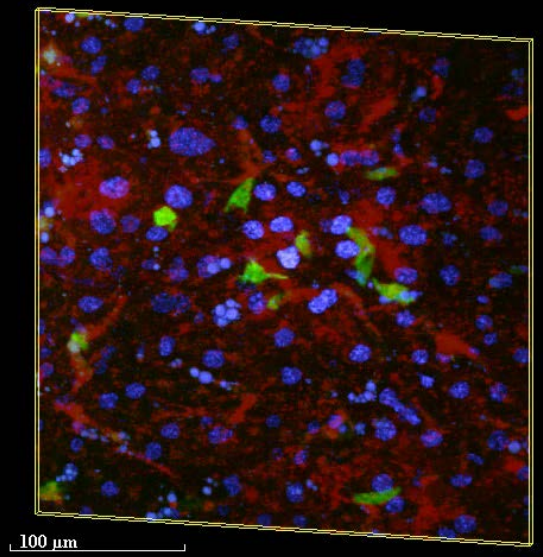
Pancreatic islets transplanted into mouse kidney
Jennifer Ryan and Natalie Stull

Sources of contrast in intravital multiphoton microscopy

- Autofluorescence
- Hoechst 33342
- Intravenous bulk probes
- Permeant bio-indicators
- Second harmonic generation
- Adoptive transfer
- Transgenic animals



GFP-expressing hematopoetic stem cells in mouse calvarium
Gosia Kamocka, Amy Zollman, Nadia Carlesso

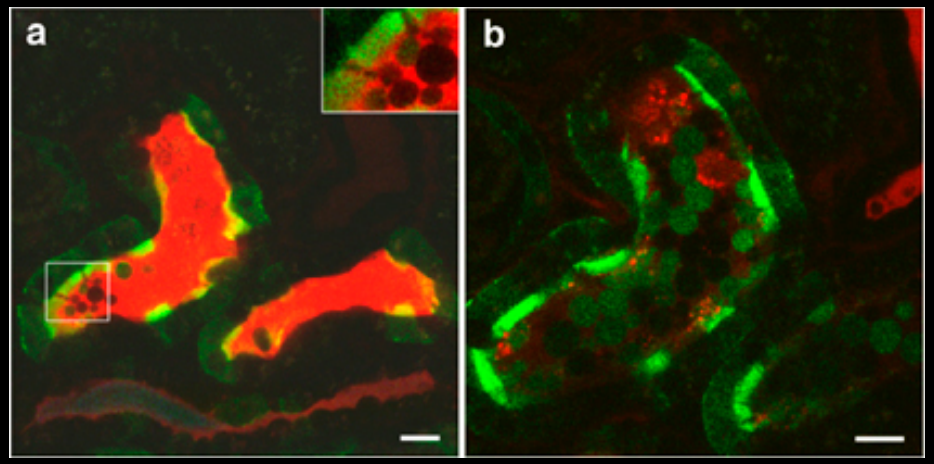


Fluorescent NKT cells in liver of GFP-Lys mouse
Cliff Babbey, Marwan Ghabril and Ken Dunn

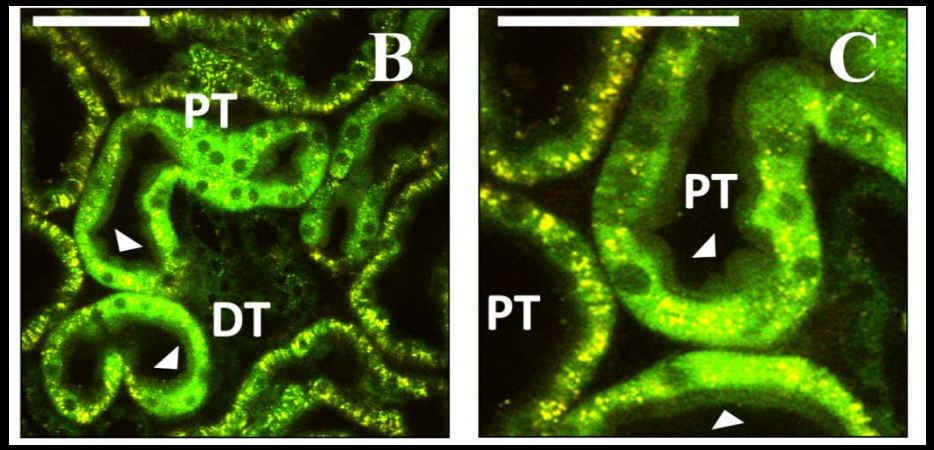
Sources of contrast in intravital multiphoton microscopy

- Autofluorescence
- Hoechst 33342
- Intravenous bulk probes
- Permeant bio-indicators
- Second harmonic generation
- Adoptive transfer
- Transgenic animals
- In vivo gene transfer

Simon Atkinson
Hydrodynamic gene delivery
Wednesday at 8:30 AM



Micropuncture injection of Adeno-GFP-actin
Ashworth et al., 2007



Hydrodynamic delivery ofAdeno-GFP-actin
Corridon et al., 2013

Sources of contrast in intravital multiphoton microscopy

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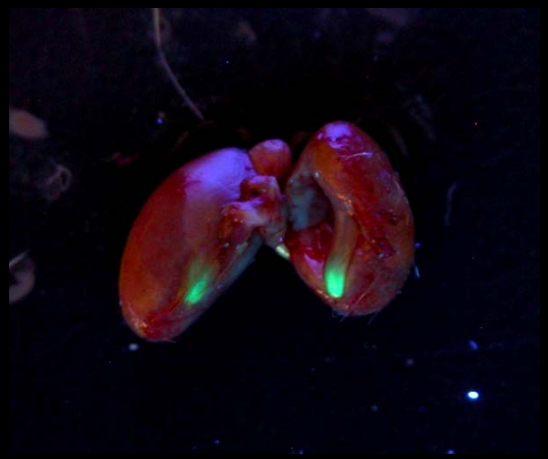
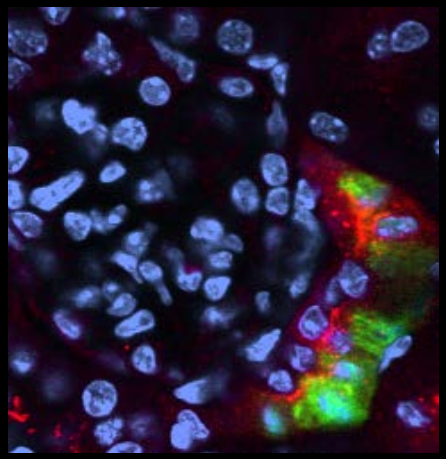
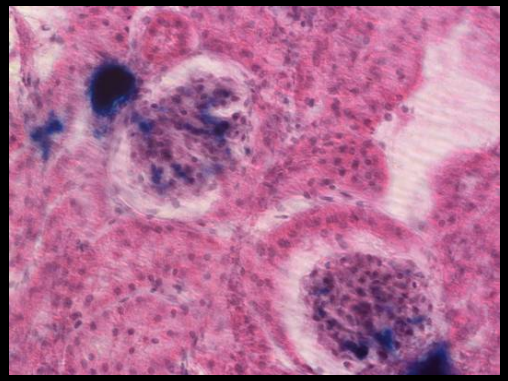
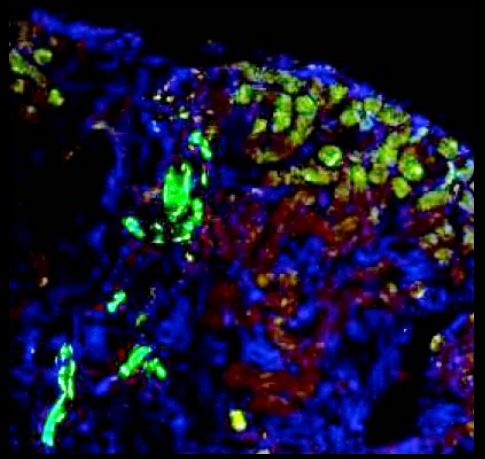




GFP expressed in renal pedicle and para-macula densa following intravenous injection of AAV9-GFP – Xiao Xiao, UNC





GFP expressed in tubules renal following subcapsular injection of AAVH48-GFP – Xiao Xiao, UNC

Xiao Xiao
AAV for in vivo gene transfer
Wednesday at 11:10 am

Further information

Websites

http://www.drbio.cornell.edu/ - Watt Webb's laboratory
http://www.microscopyu.com/ - a great general microscopy education website
http://www.loci.wisc.edu - Laboratory for Optical and Computational Instrumentation

Reviews

Girkin, J. 2003. Optical physics enables advances in multiphoton imaging. J. Phys. D: Appl. Phys. 36:R250-R258.

Helmchen, F. and W. Denk. 2005. Deep tissue two-photon microscopy. Nature Methods 2:932-940

Hoover, E. and J. Squier. 2013. Advances in multiphoton microscopy technology. Nature Photonics. 7:93-101

Zipfel, W., R. Williams and W. Webb. 2003. Nonlinear magic: multiphoton microscopy in the biosciences. Nature Biotech. 21:1369-1377.

INDIANA CENTER FOR BIOLOGICAL MICROSCOPY

The Indiana OBrien Center for Advanced Renal Microscopy